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(54) **X-RAY IMAGING DEVICE**

RÖNTGENBILDGEBUNGSVORRICHTUNG

DISPOSITIF D'IMAGERIE À RAYONS X

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Description

Technical Field

[0001] The present invention relates to an X-ray imaging device, and particularly relates to an X-ray imaging device that obtains CT (computer tomography method) images, using an X-ray imaging unit having a comparatively narrow detection area.

Background Art

[0002] There is known an X-ray imaging device for dental care that is provided with an X-ray source for irradiating a subject with X-ray flux, an X-ray imaging unit for detecting X-ray flux passing through the subject, and a turn-driving unit for turning the X-ray source and the X-ray imaging unit around the subject, and is capable of CT imaging and panorama imaging (see Patent Literature 1). The X-ray imaging device disclosed by Patent Literature 1 uses a two dimensional sensor having a wide detection area necessary for CT imaging as an X-ray imaging unit.

[0003] However, a two dimensional sensor with a wide detection area is so expensive that an X-ray imaging device becomes expensive as a whole. In this situation, an X-ray imaging device is presented that detects X-ray flux passing through a subject, by moving an X-ray imaging unit with a comparatively narrow detection area by a moving unit, and thereby functions as a virtual X-ray imaging unit for a range of the movement (Patent Literature 2).

Related Art Document

Patent Literature

[0004]

Patent Literature 1: JP 10-225455 A
Patent Literature 2: WO 2010/150719

[0005] US 2011/176717 A1, US 2010/246755 A1, US 2012/093284 A1, JP H 09 327453 A disclose different X-ray imaging devices each comprising an X-ray source for irradiating a subject with X-ray flux; an X-ray imaging unit for detecting the X-ray flux passing through the subject; a support member for supporting the X-ray source and the X-ray imaging unit; a turn-driving unit for turning the X-ray source and the X-ray imaging unit around the subject by rotating the support member; and a shifting unit for shifting a transmission part of the subject, through which the X-ray flux detected by the X-ray imaging unit passes.

[0006] In particular, US 2010/246755 A1 discloses the features of the preamble of independent claims 1 and 3.

Disclosure of the Invention

Problems to be Solved by the Invention

[0007] However, the X-ray imaging device disclosed by Patent Literature 2 needs to repeat execution of, for example, a step of imaging while moving the X-ray imaging unit by the moving unit in a certain range and a step of shift-turning the X-ray source and the X-ray imaging unit around a subject by a turn-driving unit. Consequently, when moved members such as the X-ray imaging unit and the like are temporarily stopped and restarted, it is necessary to decelerate and accelerate these moved members. Consequently, as the moving speed of the X-ray imaging unit is low immediately after the start of a movement and immediately before the stop of the movement of the X-ray imaging unit, resulting in a long total imaging time and a drop of imaging work efficiency. Further, inertia force due to acceleration or deceleration acts on moved members such as the X-ray imaging unit, which also causes the moved members to vibrate.

[0008] The present invention has been developed addressing these problems, and an object of the invention is to provide an X-ray imaging device that enables reducing cost, using an X-ray imaging unit with a comparatively narrow detection area, and reducing vibration of moved members such as the X-ray imaging unit.

Means for Solving the Problems

[0009] The invention is defined by the independent claims.

[0010] In order to solve the above-described problems, an X-ray imaging device according to the present invention includes: an X-ray source for irradiating a subject with X-ray flux; an X-ray imaging unit for detecting the X-ray flux passing through the subject; a support member for supporting the X-ray source and the X-ray imaging unit; a turn-driving unit for turning the X-ray source and the X-ray imaging unit around the subject by rotating the support member; a shifting unit for shifting a transmission part of the subject, through which the X-ray flux detected by the X-ray imaging unit passes; and a control section for controlling operation of the turn-driving unit and the shifting unit, wherein the control section executes detection of the X-ray flux passing through the subject by the X-ray imaging unit, while simultaneously executing turning of the X-ray source and the X-ray imaging unit around the subject by rotating the support member by operating the turn-driving unit, and shifting the transmission part of the subject, through which the X-ray flux detected by the X-ray imaging unit passes, by operating the shifting unit.

[0011] According to this aspect of the invention, by shifting the transmission part of the subject, through which X-ray flux L detected by the X-ray imaging unit passes, the X-ray imaging unit can function as a two dimensional X-ray imaging unit for a virtual wide range in

a range corresponding to the shifting of the transmission part. In such a manner, using, for example, an inexpensive X-ray imaging unit having a detection area in a comparatively narrow range, CT images can be obtained, which contribute to reduction in cost.

[0012] Further, while simultaneously executing turning of the X-ray source and the X-ray imaging unit around the subject and shifting of the transmission part of the subject, through which X-ray flux detected by the X-ray imaging unit passes, detection of the X-ray flux passing through the subject is executed. Thus, it is possible to reduce temporary stop and restart of moved members such as the X-ray imaging unit. As a result, as it is possible to reduce the decrease in the speed caused by operation of temporal stop and restart of the moved members from the start to end of X-ray imaging, the total imaging time becomes short, and the imaging operation efficiency is improved. Further, as it is possible to decrease acceleration and deceleration acting on the moved members, the inertia force based on the acceleration or deceleration can be decreased so that the vibration of the moved members caused by the inertia force can be decreased and the durability of the moved members can be improved.

[0013] That is, by using an X-ray imaging unit having a detection area with a comparatively narrow range, it is possible to reduce the cost, and also provide an X-ray imaging device that enables improvement of the imaging operation efficiency and reduction in vibration of moved members such as the X-ray imaging unit.

[0014] In another aspect of the invention, the control section controls operation of the turn-driving unit and the shifting unit such that neighboring transmission parts, through which the X-ray flux passes, contact with each other at both time points before and after the support member is rotated one time.

[0015] According to this aspect of the invention, as image data (projection data) necessary for generation of CT images can be effectively obtained, it is possible to further improve the imaging operation efficiency while ensuring image quality.

[0016] Still further, in another aspect of the invention, the X-ray imaging device further includes a turning-center-position horizontally moving mechanism for horizontally moving a turning center position of the support member in a direction along a line connecting the X-ray source with the X-ray imaging unit.

[0017] According to this aspect of the invention, the distance between the X-ray source and the subject can be varied by the turning-center-position horizontally moving mechanism, and it is thereby possible to adjust the largeness of FOV (field of view).

[0018] Yet further, in another aspect of the invention, a slit for restricting a range of X-ray projected from the X-ray source is arranged in order to face the X-ray imaging unit across the subject.

[0019] According to this aspect of the invention, by reducing the amount of scattering rays by arranging the slit

for restricting the range of X-ray flux, image quality can be improved.

[0020] Further, in another aspect of the invention, the shifting unit is an arcuate movement unit for arcuate moving the X-ray imaging unit around the subject in order to rotate the X-ray imaging unit around an arcuate movement central axis arranged on a line connecting the subject with the X-ray imaging unit; the support member comprises an arcuate movement arm that is axially supported around the arcuate movement central axis arranged for a turning arm turned by the turn-driving unit; the arcuate movement unit that arcuately moves the arcuate movement arm is arranged under the turning arm; wherein the X-ray source and the X-ray imaging unit are rotated around the subject by rotating the arcuate movement arm by turning the arcuate movement arm by the turn-driving unit; and the X-ray imaging unit is arcuately moved around the subject by rotating the arcuate movement arm by the arcuate movement unit.

[0021] According to this aspect of the invention, the X-ray source and the X-ray unit are arranged at the arcuate movement arm, which is a support member, and the arcuate movement arm is axially supported around the arcuate movement central axis arranged at the turning arm. Thus, the X-ray source and the X-ray imaging unit arranged at the arcuate movement arm can be turned around the subject by the turn-driving unit through the turning arm. Further, by rotating the arcuate movement arm by the arcuate movement unit, the X-ray imaging unit can be arcuately moved around the arcuate movement central axis, and the transmission part of the subject, through which the X-ray flux passes, can be shifted. Accordingly, by detecting the X-ray flux passing through the subject while arcuate movement the X-ray imaging unit by arcuate movement unit, the X-ray imaging unit can function as a two dimensional imaging unit for a virtual wide range in a range of the arcuate movement.

[0022] Still further, in another aspect of the invention, the arcuate movement central axis is provided at a position where the X-ray source is arranged.

[0023] According to this aspect of the invention, the X-ray imaging unit is arcuately moved with the X-ray source as the center, without arcuately moving the X-ray source, and it is thereby possible to restrict blurring of an image, projecting stabilized X-ray flux. Further, for example, by rotating the X-ray source in the moving direction of the X-ray imaging unit in order to match with the arcuate movement of the X-ray imaging unit, as a constant region of X-ray flux can be projected to an X-ray imaging unit, uniform X-ray flux without variation can be always projected to the subject.

[0024] Yet further, in another aspect of the invention, the shifting unit is a turning-center-position circumferential-direction-moving mechanism for moving a turning-center position of the support member along a circumferential direction of a circle having a center at a point on a line connecting the X-ray source with the X-ray imaging unit.

[0025] According to this aspect of the invention, the support member at which the X-ray source and the X-ray imaging unit are arranged is turned around the turning center position of the support member by the turn-driving unit, and the turning center position of the support member is moved by the turning-center-position circumferential-direction-moving mechanism along the circumferential direction of a circle with a center at a point on a line connecting the X-ray source with the X-ray imaging unit. Thus, the X-ray imaging unit is arcuately moved around the above-described point, and the transmission part of the subject, through which the X-ray flux passes, can be shifted. Accordingly, by detecting X-ray flux passing through the subject while arcuate movement the X-ray imaging unit by the turning-center-position circumferential-direction-moving mechanism, the X-ray imaging unit can function as a two dimensional imaging unit for a virtual wide range in a range of the arcuate movement.

[0026] Further, the shifting unit is a linearly moving unit arranged on the support member to linearly move the X-ray imaging unit.

[0027] According to this aspect of the invention, the X-ray imaging unit can be linearly moved by the linearly moving unit and the transmission part of the subject, through which the X-ray flux passes, can be thereby shifted. Accordingly, by detecting X-ray flux passing through the subject while linearly moving the X-ray imaging unit by the linearly moving unit, the X-ray imaging unit can function as a two dimensional imaging unit for a virtual wide range in a range of the linear movement.

Advantages of the Invention

[0028] According to the present invention, it is possible to provide an X-ray imaging device that enables reducing cost, using an X-ray imaging unit with a comparatively narrow detection area, and reducing vibration of moved members such as the X-ray imaging unit.

Brief Description of the Drawings

[0029]

FIG. 1 is a schematic side view of the outline configuration of an X-ray imaging device in a first embodiment according to the present invention;

FIG. 2 is a bottom view of the main part for illustration of the operation of a shifting unit;

FIG. 3 is a block diagram showing the configuration of the main control of the X-ray imaging device;

FIG. 4 is a flowchart showing the outline procedure of the operation of CT imaging;

FIG. 5 is a plan view schematically showing the view of the first turning of an X-ray source and an X-ray sensor around a subject;

FIG. 6 is a plan view schematically showing the view of the second turning of the X-ray source and the X-ray sensor around the subject;

FIG. 7 is a plan view schematically showing the view of the third turning of the X-ray source and the X-ray sensor around the subject;

FIG. 8 is a plan view schematically showing the view of the fourth turning of the X-ray source and the X-ray sensor around the subject;

FIG. 9 is a plan view schematically showing the view of the fifth turning of the X-ray source and the X-ray sensor around the subject;

FIG. 10 is a plan view of superposition of FIGs. 5-9; FIG. 11 is a plan view for illustration of a reconstructed image obtaining region where a reconstructed image can be obtained;

FIG. 12 is a side view schematically showing the outline configuration of an X-ray imaging device in a second embodiment according to the present invention;

FIG. 13 is a plan view schematically showing the periphery of a shifting unit in the second embodiment;

FIG. 14 is a perspective view schematically showing the periphery of the shifting unit in the second embodiment; and

FIG. 15 is a side view schematically showing the outline configuration of an X-ray imaging device in a third embodiment according to the present invention.

Embodiments for Carrying Out the Invention

[0030] Embodiments of the present invention will be described in detail, referring to the drawings, as appropriate.

[0031] Incidentally, the same reference symbol will be assigned to the same member or members corresponding to each other. Further, the size and the shape of a member may be schematically represented with a change or exaggeration for the convenience of illustration.

40 (First Embodiment)

[0032] FIG. 1 is a schematic side view of the outline configuration of an X-ray imaging device 1 in a first embodiment of this disclosure. FIG. 2 is a bottom view of the main part for illustration of the operation of a shifting unit 5.

[0033] As shown in FIG. 1, the X-ray imaging device 1 for dentistry in the first embodiment according to the invention is provided with a head 11 having an X-ray source 11a for irradiating a subject K with X-ray flux L, an X-ray sensor 12 as an X-ray imaging unit, an arcuate movement arm 2 as a support member for supporting the X-ray source 11a and the X-ray sensor 12, a turn-driving unit 3 such as a servo motor for rotating the arcuate movement arm 2 around an arm turning central axis C1, and a shifting unit 5 for shifting a transmission part of the subject K, through which the X-ray flux L detected by the X-ray sensor 12 passes.

[0034] Incidentally, in the present embodiment, a case of application to dentistry will be described, however, without being limited thereto, a wide variety of applications in the medical field and the like are possible.

[0035] The turn-driving unit 3 is installed on an X-Y table 15 and is configured to be able to rotationally drive a turning shaft 31 through a decelerating mechanism, not shown. The turn-driving unit 3 and the turning shaft 31 are movable in a two dimensional plane by the X-Y table 15.

[0036] The turn-driving unit 3 and X-Y table 15 are disposed in a frame 10, which horizontally extends, and the frame 10 is supported movably in the upper-lower direction with respect to a post 9, which vertically extends. Symbol 81 in FIG. 1 represents an operating section operated by an operator.

[0037] The turning shaft 31 is fixed to the upper portion of a turning-center-position horizontally moving mechanism 4, and the turning-center-position horizontally moving mechanism 4 has a connecting shaft 41 fixed on the upper surface of a turning arm 32.

[0038] The turning-center-position horizontally moving mechanism 4 has a function to horizontally move the connecting shaft 41 along the line connecting the X-ray source 11a with the X-ray sensor 12, concretely along the longitudinal direction of the turning arm 32. Herein, the turning-center-position horizontally moving mechanism 4 is provided with a nut section 42 to which the connecting shaft 41 is fixed, a male screw member 43 screw-engaged with the nut section 42, and a male-screw-member rotationally driving unit 44 such as a servo motor that rotationally drives the male screw member 43. That is, in the turning-center-position horizontally moving mechanism 4, the nut section 42 is rotated by the operation of the male-screw-member rotationally driving unit 44, and the connecting shaft 41 can be shifted along the longitudinal direction of the turning arm 32 with respect to the arm turning central axis C1 by screw transfer operation. By such a structure, it is possible to vary the distance between the X-ray source 11a and the subject K, and the size of FOV (the field of view) can be thereby adjusted.

[0039] The turn-driving unit 3 has a function to turn the arcuate movement arm 2 through the turning-center-position horizontally moving mechanism 4 and the turning arm 32 so as to rotate the X-ray source 11a and the X-ray sensor 12 around the subject K.

[0040] The shifting unit 5 has a function to shift a transmission part of the subject K, through which the X-ray flux L detected by the X-ray sensor 12 passes, substantially perpendicularly to a line connecting the X-ray source 11a with the X-ray sensor 12. In the present embodiment, the shifting unit 5 is an arcuate movement unit for arcuate moving the X-ray sensor 12 around an arcuate movement central axis C2 arranged on a line connecting the subject K with the X-ray sensor 12 to thereby arcuately move the X-ray sensor 12 around the subject K.

[0041] With such a structure, the X-ray imaging device

1 turns the turning arm 32 by the turn-driving unit 3 to thereby rotate the arcuate movement arm 2 and thereby rotate the X-ray source 11a and the X-ray sensor 12 around the subject K, and can arcuately move the X-ray sensor 12 by rotating the arcuate movement arm 2 around the subject K by the shifting unit 5.

[0042] The X-ray source 11a is arranged at a support member 11b fixed downward from the arcuate movement arm 2. Accordingly, the projection direction of X-ray flux L projected from the X-ray source 11a varies with the rotation of the arcuate movement arm 2, and the X-ray sensor 12 also arcuately moves, in synchronization in order to follow the projection direction of the X-ray flux L (see FIG. 2).

[0043] Further, a slit 13 for restricting the range of X-ray flux L projected from the X-ray source 11a is arranged on the subject K side of the head 11 in order to face the X-ray sensor 12 across the subject K. The X-ray flux L having been narrowed by the slit 13 passes through the subject K and is detected by the X-ray sensor 12. By arranging the slit 13, the amount of scattering rays can be reduced so that the image quality can be improved. The slit 13 may be arranged in order to extend downward from the arcuate movement arm 2.

[0044] The X-ray sensor 12 can be configured by the use of an image sensor having a vertically longitudinal detection area in a comparatively narrow range, such as a CMOS sensor, a CCD sensor, a CdTe sensor, or the like to detect X-ray flux L passing through the subject K.

[0045] For example, CMOS sensors feature low cost and low power consumption. CCD sensors feature a high resolution, and allow selection of an optical image sensor, based on specifications required for an X-ray imaging device.

[0046] The arcuate movement arm 2 is axially and rotatably supported around an axial member 21 having the arcuate movement central axis C2 arranged at the turning arm 32 turned by the turn-driving unit 3. The arcuate movement central axis C2 is herein arranged coaxially with the X-ray source 11a of the head 11 arranged at the arcuate movement arm 2. By such a structure, the X-ray sensor 12 is arcuately moved with the X-ray source 11a as the center, without arcuately moving the X-ray source 11a, and it is thereby possible to restrict blurring of an image, projecting stabilized X-ray flux L. Further, for example, by rotating the X-ray source 11a in the moving direction of the X-ray sensor 12 in order to match with the arcuate movement of the X-ray sensor 12, as a constant region of X-ray flux can be projected to an X-ray imaging unit, uniform X-ray flux without variation can be always projected to the subject K.

[0047] The arcuate movement arm 2 is provided with the X-ray source 11a, the slit 13, and the X-ray sensor 12 on a line. Thus, it is possible to narrow the X-ray flux L projected from the X-ray source 11a by the slit 13 to project a constant region of the X-ray flux L to the X-ray sensor 12. Accordingly, it is possible to efficiently irradiate the subject K always with a uniform X-ray flux L with-

out variation.

[0048] As shown in FIG. 1 and FIG. 2, the shifting unit 5 is provided with a rotating-arm rotationally driving unit 51 such as a servo motor installed at the turning arm 32, a rotation shaft 52 connected to the rotating-arm rotationally driving unit 51, a rotating arm 53 to which one end portion the tip end of the rotation shaft 52 is fixed, a driving pin 54 arranged at the other end portion of the rotating arm 53, and a guide groove 55 formed on the arcuate movement arm 2 in order to engage with the driving pin 54.

[0049] With such a structure, when the shifting unit 5 rotates the rotating arm 53 around the rotation shaft 52 clockwise R1 in FIG. 2, the arcuate movement arm 2 arcuately moves around the arcuate movement central axis C2 from a central position P0 to a gradient position P1 in FIG. 2. When the shifting unit 5 rotates likewise the rotating arm 53 around the rotation shaft 52 counterclockwise R2 in FIG.2, the arcuate movement arm 2 arcuately moves around the arcuate movement central axis C2 from the central position P0 to a gradient position P2 in FIG. 2.

[0050] In such a manner, by arcuate movement the arcuate movement arm 2 around the arcuate movement central axis C2, it is possible to arcuately move the slit 13 and the X-ray sensor 12 arranged at the arcuate movement arm 2.

[0051] Though not shown, the X-Y table 15 is constructed by combination of a linearly moving guide arranged movably in X-axial direction and a linearly moving guide arranged movably in Y-axial direction, the linearly moving guides being arranged in order to be perpendicular to each other in the horizontal direction.

[0052] Being provided with the X-Y table 15, as the X-ray imaging device 1 can translate the arcuate movement arm 2 in a horizontal two dimensional plane, the X-ray imaging device 1 functions as an imaging device capable of generating both CT images and panorama images.

[0053] That is, in using the X-ray imaging device 1 as a CT imaging device, the X-Y table 15 is fixed, and the position of the arm rotation central axis C1 in the horizontal plane is thereby fixed, which enables CT imaging. On the other hand, in using the X-ray imaging device 1 as a usual panorama imaging device, in a state that the arcuate movement arm 2 is fixed without being arcuately moved, the arcuate movement arm 2 and the turning arm 32 are integrally translated by the X-Y table 15 in a horizontal two dimensional plane, which enables panorama imaging.

[0054] FIG. 3 is a block diagram showing the configuration of the main control of the X-ray imaging device 1.

[0055] As shown in FIG. 3, the X-ray imaging device 1 is provided with a control section 8 for performing integral control of the entire X-ray imaging device 1. For example, the control section 8 performs control of the operation of X-ray imaging of the subject K. That is, the control section 8 controls the irradiation operation of the X-ray source

11a, and executes detection of X-ray flux L (see FIG. 1) passing through the subject K by the X-ray sensor 12. Further, the control section 8 controls the operation of the turn-driving unit 3, the rotating-arm rotationally driving unit 51 (see FIG. 1) of the shifting unit 5 (see FIG.1), and the male-screw-member rotationally driving unit 44.

[0056] In the present embodiment, the control section 8 is configured to control the operation of X-ray imaging of the subject K (see FIG. 1) while simultaneously executing turning of the X-ray source 11a and the X-ray sensor 12 around the subject K and shifting a transmission part of the subject K, through which the X-ray flux L (see FIG. 1) detected by the X-ray sensor 12 passes.

[0057] The X-ray imaging device 1 is also provided with an image processing section 82, an external storage device 83, and a display section 84, which are connected to the control section 8. The image processing section 82 performs image processing of image data (projection data) detected and obtained by the X-ray sensor 12, and generates various images such as CT imagers and panorama images. The external storage device 83 is for example a hard disk device or an optical disk device, and can store various images. The display section 84 is for example an LCD (liquid crystal display) and can display various images.

[0058] Further, via an operating section 81, it is possible to switch various imaging modes such as CT imaging and panorama imaging, setting of the shift amount for shifting a transmission part of the subject K, through which the X-ray flux L detected by the X-ray sensor 12 passes.

[0059] The operation of such configured X-ray imaging device 1 will be described, referring to FIGs. 4 toll. FIG. 4 is a flowchart showing the outline procedure of the operation of CT imaging. FIGs. 5 to 9 are plan views schematically showing the first to fifth turnings of the X-ray source and the X-ray sensor around the subject.

[0060] As shown in FIG. 4, if an operator operates the operating section 81 (see FIG. 1 and FIG. 3), X-ray imaging processing is executed by the X-ray imaging device 1 (step S1). Herein, a case where CT imaging is performed will be described.

[0061] In the present embodiment, the control section 8 (see FIG. 3) executes detection of X-ray flux L, which has passed through the subject K, by the X-ray sensor 12, while simultaneously executing: turning of the X-ray source 11a and the X-ray sensor 12 around the subject K by rotating the arcuate movement arm 2 by operation of the turn-driving unit 3 (see FIG. 1); and shifting a transmission part of the subject K, through which the X-ray flux L detected by the X-ray sensor 12 passes, by operation of the shifting unit 5 (see FIG. 1).

[0062] Concretely, as shown in FIG. 5, first, X-ray flux L projected from the X-ray source 11a located at a position P10 (position at 0 degree), in FIG. 5, in the first turn passes through the first region R1, in FIG. 5, which corresponds to the outermost side (the lowest side in FIG. 5) of the subject K and is detected by the X-ray sensor

12. In the first turn, the X-ray source 11a and the X-ray sensor 12 are turned from this state around the subject K such that the X-ray source 11a rotationally moves by 360 degrees through the positions P11 to P15, and simultaneously, the transmission part of the subject K, through which the X-ray flux L detected by the X-ray sensor 12 passes, is gradually shifted upward from the first region R1 in FIG. 5 to the second region R2 in FIG. 6.

[0063] Likewise, in the second turning, as shown in FIG. 6, the X-ray source 11a located at the position P20 (0 degree position) in FIG. 6 rotationally moves by 360 degrees to the position P26 (see FIG. 7) through the positions P21 to P25, and simultaneously, the transmission part of the subject K, through which the X-ray flux L detected by the X-ray sensor 12 passes, is gradually shifted upward from the second region R2 in FIG. 6 to the third region R3 in FIG. 7. In the third turning, as shown in FIG. 7, the X-ray source 11a located at the position P30 (0 degree position) in FIG. 7 rotationally moves by 360 degrees to the position P36 through the positions P31 to P35, and simultaneously, the transmission part of the subject K, through which the X-ray flux L detected by the X-ray sensor 12 passes, is gradually shifted upward from the third region R3 in FIG. 7 to the fourth region R4 in FIG. 8. In the fourth turning, as shown in FIG. 8, the X-ray source 11a located at the position P40 (0 degree position) in FIG. 8 rotationally moves by 360 degrees to the position P46 (see FIG. 9) through the positions P41 to P45, and simultaneously, the transmission part of the subject K, through which the X-ray flux L detected by the X-ray sensor 12 passes, is gradually shifted upward from the fourth region R4 in FIG. 7 to the fifth region R5 in FIG. 9. In the fifth turning, as shown in FIG. 9, the X-ray source 11a located at the position P50 (0 degree position) in FIG. 9 rotationally moves by 360 degrees to the position P56 through the positions P51 to P55, and simultaneously, the transmission part of the subject K, through which the X-ray flux L detected by the X-ray sensor 12 passes, is gradually shifted upper than the fifth region R5 in FIG. 9. Incidentally, in FIG. 9, the transmission part at the position P56 is not shown.

[0064] FIG. 10 is a plan view of superposition of FIGs. 5-9. FIG. 11 is a plan view for illustration of the reconstructed image obtaining region where a reconstructed image can be obtained.

[0065] As shown in FIG. 10, it is proved that, for the same angular position (positions V0 to V5) in the respective turnings, the X-ray source 11a is located at the same position, and the position of the X-ray sensor 12 arcuately moves, in other words, shifts in every turning with the position of the X-ray source 11a as the center. That is, FIG. 10 corresponds to a plan view schematically showing the view of a case of turning a virtual X-ray sensor 12v once around the subject K, the virtual X-ray sensor 12v being in a wide range virtually formed by the shift of the X-ray sensor 12. In FIG. 10, the region of the subject K shows FOV (field of view).

[0066] Further, in the present embodiment, the control

section 8 controls the operation of the turn-driving unit 3 and the shifting unit 5 such that neighboring transmission parts, through which the X-ray flux L passes, contact with each other at both time points before and after the arcuate movement arm 2 makes one rotation through the turning arm 32. Herein, the shift amount S of the X-ray sensor 12 made by one rotation of the arcuate movement arm 2 is almost equal to the width (effective width) W of the X-ray sensor 12. In the example in FIG. 10, while the X-ray sensor 12 is shifted, the arcuate movement arm 2 is rotated in five times, which is the number of rotations computed as (the width Wv of the virtual X-ray sensor 12v) ÷ (the width W of the X-ray sensor 12) = 5 times. By such an arrangement, image data (projection data) necessary for generation of CT images can be effectively obtained, which enables ensuring image quality and a further improvement of the imaging efficiency.

[0067] Incidentally, in the present embodiment, during turning of the X-ray source 11a and the X-ray sensor 12 around the subject K, the transmission part of the subject K, through which the X-ray flux L detected by the X-ray sensor 12 passes, shifts. Consequently, in the example shown in FIG. 11, in the region corresponding to the width of the X-ray sensor 12 at the outer circumferential portion of the FOV, it is not possible to obtain image data (projection data) from all directions and it is difficult to generate reconstructed image such as CT images. Accordingly, the reconstructed image obtaining region RA (see FIG. 11) is a region formed by removing the outer circumferential portion corresponding to the width of the X-ray sensor 12 from the FOV.

[0068] Returning to step S2 in FIG. 4, when the image data (projection data) obtained by CT imaging is transmitted to the image processing section 82, the control section 8 controls the image processing section 82 to perform certain processing on the image data (projection data) and thereby generate a CT image.

[0069] Subsequently, the control section 8 controls the display section 84 to display the generated CT image (step S3). Further, the generated CT image can be stored in the external storage device 83, as necessary.

[0070] In an embodiment as described above, by shifting the transmission part of the subject K, through which the X-ray flux L detected by the X-ray sensor 12 passes, the X-ray sensor 12 can function as a two dimensional X-ray imaging unit for a virtual wide range in a range corresponding to the shifting of the transmission part. In such a manner, using for example an inexpensive X-ray sensor 12 having a detection area in a comparatively narrow range, CT images can be obtained, which contribute to reduction in cost.

[0071] While simultaneously executing turning of the X-ray source 11a and the X-ray sensor 12 around the subject K and shifting of the transmission part of the subject K, through which the X-ray flux L detected by the X-ray sensor 12 passes, detection of the X-ray flux L passing through the subject K is executed, and it is thereby possible to reduce temporary stop and restart of moved

members such as the X-ray sensor 12. As a result, as it is possible to reduce decrease in the speed caused by operation of temporal stop and restart of the moved members from the start to the end of X-ray imaging, the total imaging time becomes short, and the imaging operation efficiency is improved. Further, as it is possible to decrease the acceleration and deceleration acting on the moved members, the inertia force based on the acceleration or deceleration can be decreased so that the vibration of the moved members caused by the inertia force can be decreased and the durability of the moved members can be improved.

[0072] That is, by using an X-ray sensor 12 having a detection area in comparatively narrow range, it is possible to reduce the cost, and also provide an X-ray imaging device 1 that enables improvement of imaging operation efficiency and reduction in vibration of moved members such as the X-ray sensor 12.

[0073] Further, in the present embodiment, the X-ray source 11a and the X-ray sensor 12 are arranged at the arcuate movement arm 2, which is a support member, and the arcuate movement arm 2 is axially supported around the arcuate movement central axis C2 arranged at the turning arm 32. Thus, the X-ray source 11a and the X-ray sensor 12 arranged at the arcuate movement arm 2 can be turned around the subject K by the turn-driving unit 3 through the turning arm 32. Further, by rotating the arcuate movement arm 2 by arcuate movement unit as the shifting unit 5, the X-ray sensor 12 can be arcuately moved around the arcuate movement central axis C2, and the transmission part of the subject K, through which the X-ray flux L passes, can be thereby shifted. Accordingly, by detecting the X-ray flux L passing through the subject K while arcuate movement the X-ray sensor 12 by arcuate movement unit, the X-ray sensor 12 can function as a two dimensional imaging unit with a virtual wide range in a range of the arcuate movement.

(Second Embodiment)

[0074] FIG. 12 is a side view schematically showing the outline configuration of an X-ray imaging device 1a in a second embodiment according to the present invention. FIG. 13 is a plan view schematically showing the periphery of a shifting unit in the second embodiment. FIG. 14 is a perspective view schematically showing the periphery of the shifting unit in the second embodiment. The X-ray imaging device 1a in the second embodiment will be described on points different from the above-described X-ray imaging device 1 in the first embodiment.

[0075] As shown in FIG. 12, in the X-ray imaging device 1a in the second embodiment of the present invention, a shifting unit 6 is different from the shifting unit 5 in the first embodiment in that the shifting unit 6 is a turning-center-position circumferential-direction-moving mechanism that moves the turning central position of a turning arm 32 as a support member along the circumferential direction of a circle with a center at a point on a line con-

necting the X-ray source 11a with the X-ray sensor 12 being herein a point on an arcuate movement central axis C2, which is a vertical shaft going through the X-ray source 11a. Incidentally, in the second embodiment, a turning-center-position horizontally moving mechanism 4 as one in the first embodiment is omitted, however, may be installed.

[0076] A turning shaft 31 is fixed to the upper portion of the shifting unit 6, and has a connecting shaft 61 fixed to the upper surface of the turning arm 32.

[0077] The shifting unit 6 has a function to move the connecting shaft 61 around the arcuate movement central axis C2 to thereby arcuately move the turning center position of the turning arm 32 as a result. Herein, the turning center position of the turning arm 32 corresponds to the intersection point on the turning arm 32 with the arm turning central axis C1.

[0078] As shown in FIGs. 12 to 14, the shifting unit 6 is provided with a slide gear 62 in an arcuate shape to which the connecting shaft 61 is fixed, a pinion gear 63 engaged with the slide gear 62, a pinion gear rotational-driving unit 64 such as a servo motor for rotationally driving the pinion gear 63, and a guide member 65 for guiding the circumferentially directed movement (arcuate movement) of the slide gear 62. Inner teeth are formed inside the slide gear 62, with the arcuate movement central axis C2 as the center. That is, in the shifting unit 6, the pinion gear 63 is rotated by the operation of the pinion gear rotational-driving unit 64, and the gear force moves the slide gear 62 so that the connecting shaft 61 can be shifted along the circumferential direction of a circle with a radius r (see FIG. 14) with the arcuate movement central axis C2 as the center. Incidentally, symbol 66 in FIG. 13 and FIG. 14 represents a guide groove for guiding the movement of the connecting shaft 61.

[0079] In the second embodiment, the turning arm 32 as a support member, the turning arm 32 being provided with the X-ray source 11a and the X-ray sensor 12, is turned around the turning center position of the turning arm 32 by the turn-driving unit 3, and the turning center position of the turning arm 32 is moved along the circumferential direction with the arcuate movement central axis C2 as the center by the shifting unit 6, which is a turning-center-position circumferential-direction-moving mechanism. Thus, the X-ray sensor 12 is arcuately moved around the arcuate movement central axis C2, and the transmission part of the subject K, through which the X-ray flux L passes, can be shifted. Accordingly, by detecting X-ray flux L passing through the subject K while arcuate movement the X-ray sensor 12 by the shifting unit 6, which is a turning-center-position circumferential-direction-moving mechanism, the X-ray sensor 12 can function as a two dimensional imaging unit in a virtual wide range in a range of the arcuate movement.

[0080] Accordingly, also in the second embodiment, operation and advantages similar to those in the above-described first embodiment can be obtained.

(Third Embodiment)

[0081] FIG. 15 is a side view schematically showing the outline configuration of an X-ray imaging device 1b in a third embodiment according to the present invention. In the following, the X-ray imaging device 1b in the third embodiment will be described on points different from the above-described X-ray imaging device 1 in the first embodiment.

[0082] As shown in FIG. 15, in the X-ray imaging device 1b in the third embodiment according to the present invention, a shifting unit 7 is different from the shifting unit 5 in the first embodiment in that the shifting unit 7 is a linear moving unit that is provided at a turning arm 32 as a support member and linearly moves the X-ray sensor 12. Incidentally, in the third embodiment, a turning-center-position horizontally moving mechanism 4 as one in the first embodiment is omitted, however, may be installed.

[0083] While, in the above-described first and second embodiments, the X-ray sensor 12 is arcuately moved around the arcuate movement central axis C2, the third embodiment corresponds to a case that the arcuate movement central axis C2 (see FIG. 1 and FIG. 12) is set at a distance extremely far from the subject K.

[0084] The shifting unit 7, which is a linearly moving unit for linearly moving, is provided with a linearly moving unit 70 for linearly moving the X-ray sensor 12, and a linearly moving unit 75 for linearly moving a slit 13 for restricting the range of X-ray flux L projected from the X-ray source 11a. The linearly moving unit 70 is arranged at the turning arm 32. The linearly moving unit 75 is arranged at the turning arm 32 through a support member 11b, however, may be arranged directly at the turning arm 32.

[0085] The linearly moving unit 70 is provided with a guide rail 71 arranged along the direction of linear moving, a holder 72 reciprocally movably attached along the guide rail 71, a nut section 73 fixed to the holder 72, a male screw member 74 screw-engaged with the nut section 73, and a male-screw-member rotationally driving unit not shown such as a servo motor that rotationally drives the male screw member 74.

[0086] Further, the linearly moving unit 75 for linearly moving the slit 13 is likewise provided with a guide rail 76, a holder 77, a nut section 78, a male screw member 79, and a male-screw-member rotationally driving unit not shown such as a servo motor that rotationally drives the male screw member 79. The linearly moving unit 70 and the linearly moving unit 75 are controlled in order to move in synchronization with each other.

[0087] In the third embodiment, the X-ray sensor 12 can be linearly moved by the shifting unit 7, which is a unit for linearly moving, and the transmission part of the subject K, through which the X-ray flux L passes, can be thereby shifted. Accordingly, by detecting X-ray flux L passing through the subject K while linearly moving the X-ray sensor 12 by the shifting unit 7, which is a unit for

linearly moving, the X-ray sensor 12 can function as a two dimensional imaging unit in a virtual wide range in a range of the linear movement.

[0088] Accordingly, also in the third embodiment, operation and advantages similar to those in the above-described first embodiment can be obtained.

[0089] The present invention has been described above, based on embodiments, however, the disclosure is not limited to the structures described in the above-described embodiments, and modifications and changes of the structures can be made, as appropriate, in a range without departing from the scope of the disclosure, including combination or selection, as appropriate, of the structures described in the above-described embodiments.

[0090] For example, in the above-described embodiments, the shift amount S by which the X-ray sensor 12 shifts when the arcuate movement arm 2 makes one rotation was set in order to be substantially equal to the width (effective width) W of the X-ray sensor 12, however, the disclosure is not limited thereto. The shift amount S can be set, as appropriate, depending on a required resolution of a CT image or the like. For example, the shift amount S may be set in order to form a gap between neighboring transmission parts, through which the X-ray flux L passes, or may be set such that the neighboring transmission parts partially overlap with each other, at both time points before and after the arcuate movement arm 2 make one rotation. Further, the shift amount S can also be set such that the shift amount S, by which the X-ray sensor 12 shifts when the arcuate movement arm 2 makes for example a half rotation, is substantially equal to the width (effective width) W of the X-ray sensor 12.

[0091] Further, in the above-described embodiments, the number of times of turning the arcuate movement arm 2 in X-ray imaging was set to for example five times, however, arrangement may be made such that the number of times can be set in order to match the necessity via the operating section 81.

[0092] Further, the shifting units 5 to 7 are examples of shifting units for shifting the transmission part of the subject K, through which the X-ray flux L detected by the X-ray sensor 12 passes, and shifting units are not limited to the structures in the above-described first to third embodiments. For example, in the second embodiment, the X-ray sensor 12 is arcuately moved around the X-ray source 11a, however, arrangement may be made such that the X-ray source 11a is arcuately moved around the X-ray sensor 12. In this case also, it is possible to shift the transmission part of the subject K, through which the X-ray flux L passes. Further, the shifting unit 7 in the third embodiment is not particularly limited to the structure described above, and it is also possible to implement a unit for linearly moving by adopting a straight rack instead of the slide gear 62 in an arcuate shape in the second embodiment shown in FIGs. 12 to 14.

[0093] Still further, in the first and second embodiments, the arcuate movement central axis C2 was ar-

ranged at the X-ray source 11a, however, without being limited thereto, the arcuate movement central axis C2 may be arranged on a line connecting the subject K with the X-ray sensor 12. Further, in the present embodiment, the slit 13 for restricting the range of X-ray flux L was arranged, however, without being limited thereto, the disclosure can be carried out even without providing the slit 13.

[0094] Yet further, in the above-described embodiments, CT image generating processing (step S2) is executed after the X-ray imaging processing (step S1) is completed, however, the disclosure is not limited thereto, and generation of CT images may be sequentially executed from a region in which image reconstructing has become possible during X-ray imaging processing. By such an arrangement, the total time of CT imaging operation can be shortened.

[0095] An X-ray imaging device may also be used for medical care other than dental care. Further, the object of imaging may be other than human being, and accordingly, an X-ray imaging device may be used for testing of a thing.

Description of Reference Symbols

[0096]

- 1, 1a, 1b: X-ray imaging device
- 2: arcuate movement arm (support member)
- 3: turn-driving unit
- 4: turning-center-position horizontally moving mechanism
- 5 - 7: shifting unit
- 8: control section
- 11a: X-ray source
- 12: X-ray sensor
- 13: slit
- 32: turning arm (support member)
- 70: linearly moving unit
- C1: arm turning central axis
- C2: arcuate movement central axis
- K: subject
- L: X-ray flux
- R1 - R5: region of transmission part

Claims

1. An X-ray imaging device (1a), comprising:
 - an X-ray source (11a) for irradiating a subject (K) with X-ray flux (L);
 - an X-ray imaging unit (12) for detecting the X-ray flux (L) passing through the subject (K);
 - a support member (11b) for supporting the X-ray source (11a) and the X-ray imaging unit (12);
 - a turn-driving unit (3) for turning the X-ray source (11a) and the X-ray imaging unit (12) around the

subject (K) by rotating the support member (11b);

a shifting unit (6) for shifting a transmission part (R1, R2, R3, R4, R5) of the subject (K), through which the X-ray flux (L) detected by the X-ray imaging unit (12) passes; and

a control section (8) for controlling operation of the turn-driving unit (3) and the shifting unit (6), wherein the control section (8) is configured so that it executes detection of the X-ray flux (L) passing through the subject (K) by the X-ray imaging unit (12), while simultaneously executing turning of the X-ray source (11a) and the X-ray imaging unit (12) around the subject (K) by rotating the support member (11b) by operating the turn-driving unit (3), and shifting the transmission part of the subject (K), through which the X-ray flux (L) detected by the X-ray imaging unit (12) passes, by operating the shifting unit (6),

characterized by

the shifting unit being a turning-center-position circumferential-direction-moving mechanism (6) for moving a turning-center position of the support member (11b) along a circumferential direction of a circle having a center at a point on a line connecting the X-ray source (11a) with the X-ray imaging unit (12), wherein the shifting unit (6) is provided with a slide gear (62) in an arcuate shape to which a connecting shaft (61) is fixed, a pinion gear (63) engaged with the slide gear (62), a pinion gear rotational-driving unit (64), such as a servo motor, for rotationally driving the pinion gear (63), and a guide member (65) for guiding the circumferentially directed movement of the slide gear (62), wherein the connecting shaft (61) is fixed to the upper surface of a turning arm (32) turnable by the turn-driving unit (3) and having an arcuate movement central axis (C2), wherein a turning shaft (31) is fixed to the upper portion of the shifting unit (6), wherein inner teeth are formed inside the slide gear (62), with the arcuate movement central axis (C2) as the center so that in the shifting unit (6), the pinion gear (63) is rotated by the operation of the pinion gear rotational-driving unit (64), and the gear force moves the slide gear (62) so that the connecting shaft (61) can be shifted along the circumferential direction of a circle with a radius (r) with the arcuate movement central axis (C2) as the center;

a guide groove (66) for guiding the movement of the connecting shaft (61).

2. The X-ray imaging device (1a) according to claim 1, wherein a slit (13) for restricting a range of X-ray projected from the X-ray source (11a) is arranged in order to face the X-ray imaging unit (12) across the

subject (K).

3. An X-ray imaging device (1b),
 an X-ray source (11a) for irradiating a subject (K) with X-ray flux (L);
 an X-ray imaging unit (12) for detecting the X-ray flux (L) passing through the subject (K);
 a support member (11b) for supporting the X-ray source (11a) and the X-ray imaging unit (12);
 a turn-driving unit (3) for turning the X-ray source (11a) and the X-ray imaging unit (12) around the subject (K) by rotating the support member (11b);
 a shifting unit (7) for shifting a transmission part (R1, R2, R3, R4, R5) of the subject (K), through which the X-ray flux (L) detected by the X-ray imaging unit (12) passes;
 a slit (13) for restricting a range of X-ray projected from the X-ray source (11a) arranged in order to face the X-ray imaging unit (12) across the subject (K); and
 a control section (8) for controlling operation of the turn-driving unit (3) and the shifting unit (7), wherein the control section (8) is configured so that it executes detection of the X-ray flux (L) passing through the subject (K) by the X-ray imaging unit (12), while simultaneously executing turning of the X-ray source (11a) and the X-ray imaging unit (12) around the subject (K) by rotating the support member (11b) by operating the turn-driving unit (3), and shifting the transmission part of the subject (K), through which the X-ray flux (L) detected by the X-ray imaging unit (12) passes, by operating the shifting unit (7),
characterized by
 the shifting unit (7) being a linearly moving unit (70) arranged at the support member (11b) to linearly move the X-ray imaging unit (12),
 the linearly moving unit (70) is provided with a guide rail (71) arranged along a direction of linear moving, a holder (72) reciprocally movably attached along the guide rail (71), a nut section (73) fixed to the holder (72), a male screw member (74) screw-engaged with the nut section (73), and a male-screw-member rotationally driving unit, such as a servo motor, that rotationally drives the male screw member (74);
 a linearly moving unit (75) for linearly moving said slit (13), the linearly moving unit (75) being arranged directly at a turning arm (32) or through a support member (11b), wherein the turning arm (32) is turnable by the turn-driving unit (3) and has an arcuate movement central axis (C2);
 wherein the linearly moving unit (75) for linearly moving the slit (13) is provided with a guide rail (76), a holder (77), a nut section (78), a male screw member (79), and a male-screw-member rotationally driving unit, such as a servo motor, that rotationally drives the male screw member (79), the linearly moving

unit (70) and the linearly moving unit (75) being controllable for moving in synchronization with each other.

4. The X-ray imaging device (1a, 1b) according to anyone of the previous claims, wherein the control section (8) controls operation of the turn-driving unit (3) and the shifting unit (6, 7) such that neighboring transmission parts, through which the X-ray flux (L) passes, contact with each other at both time points before and after the support member (11b) is rotated one time.

15 Patentansprüche

1. Eine Röntgenbildgebungsvorrichtung (1a), aufweisend:
 eine Röntgenquelle (11a) zum Bestrahlen eines Subjekts (K) mit einem Röntgenstrahlenfluss (L);
 eine Röntgenbildgebungseinheit (12) zum Erfassen des Röntgenstrahlenflusses (L), der durch das Subjekt (K) verläuft;
 ein Tragelement (11b) zum Tragen der Röntgenquelle (11a) und der Röntgenbildgebungseinheit (12);
 eine Drehantriebseinheit (3) zum Drehen der Röntgenquelle (11a) und der Röntgenbildgebungseinheit (12) um das Subjekt (K) durch Drehen des Tragelements (11b);
 eine Verschiebeeinheit (6) zum Verschieben eines Übertragungsteils (R1, R2, R3, R4, R5) des Subjekts (K), durch das der von der Röntgenbildgebungseinheit (12) erfasste Röntgenstrahlenfluss (L) verläuft; und
 einen Steuerungsabschnitt (8) zum Steuern des Betriebs der Drehantriebseinheit (3) und der Verschiebeeinheit (6),
 wobei der Steuerungsabschnitt (8) derart konfiguriert ist, dass er die Erfassung des Röntgenstrahlenflusses (L), der durch das Subjekt (K) verläuft, durch die Röntgenbildgebungseinheit (12) durchführt, während er gleichzeitig ein Drehen der Röntgenquelle (11) und der Röntgenbildgebungseinheit (12) um das Subjekt (K) durch Drehen des Tragelements (11b) durch Betreiben der Drehantriebseinheit (3) und ein Verschieben des Übertragungsteils des Subjekts (K), durch den der von der Röntgenbildgebungseinheit (12) erfasste Röntgenstrahlenfluss (L) verläuft, durch Betreiben der Verschiebeeinheit (6) durchführt,
dadurch gekennzeichnet, dass
 die Verschiebeeinheit ein Drehzentrumspositions-Umfangsrichtungs-Bewegungsmechanismus (6) ist zum Bewegen einer Drehzentrumsp-

- position des Tragelements (11b) entlang einer Umfangsrichtung eines Kreises, der ein Zentrum an einem Punkt auf einer Linie, die die Röntgenquelle (11a) mit der Röntgenbildungseinheit (12) verbindet, aufweist, wobei die Verschiebeeinheit (6) mit einem Gleitgetriebe (62) in einer Bogenform, an dem eine Verbindungswelle (61) befestigt ist, einem Ritzel (63), das mit dem Gleitgetriebe (62) in Eingriff steht, einer Ritzel-Drehantriebseinheit (64), wie einem Servomotor, für den Drehantrieb des Ritzels (63) und einem Führungselement (65) zum Führen der in Umfangsrichtung verlaufenden Bewegung des Gleitgetriebes (62) bereitgestellt wird, wobei die Verbindungswelle (61) an der Oberseite eines Dreharms (32), der von der Drehantriebseinheit (3) gedreht werden kann und eine Mittelachse (C2) zur bogenförmigen Bewegung aufweist, befestigt ist, wobei eine Drehwelle (31) am oberen Abschnitt der Verschiebeeinheit (6) befestigt ist, wobei innere Zähne im Gleitgetriebe (62) mit der Mittelachse (C2) zur bogenförmigen Bewegung als Zentrum ausgebildet sind, so dass in der Verschiebeeinheit (6) das Ritzel (63) durch den Betrieb der Ritzel-Drehantriebseinheit (64) gedreht wird, und wobei die Zahnradkraft das Gleitgetriebe (62) bewegt, so dass die Verbindungswelle (61) entlang der Umfangsrichtung eines Kreises mit einem Radius (r) mit der Mittelachse (C2) zur bogenförmigen Bewegung als Zentrum verschoben werden kann; eine Führungsnut (66) zum Führen der Bewegung der Verbindungswelle (61).
2. Die Röntgenbildgebungsvorrichtung (1a) nach Anspruch 1, wobei ein Schlitz (13) zum Beschränken eines Bereichs eines von der Röntgenquelle (11a) projizierten Röntgenstrahls angeordnet ist, um der Röntgenbildungseinheit (12) über die Erstreckung des Subjekts (K) zugewandt zu sein.
 3. Eine Röntgenbildgebungsvorrichtung (1b), eine Röntgenquelle (11a) zum Bestrahlen eines Subjekts (K) mit einem Röntgenstrahlenfluss (L); eine Röntgenbildungseinheit (12) zum Erfassen des Röntgenstrahlenflusses (L), der durch das Subjekt (K) verläuft; ein Tragelement (11b) zum Tragen der Röntgenquelle (L) und der Röntgenbildungseinheit (12); eine Drehantriebseinheit (3) zum Drehen der Röntgenquelle (11a) und der Röntgenbildungseinheit (12) um das Subjekt (K) durch Drehen des Tragelements (11b); eine Verschiebeeinheit (7) zum Verschieben eines Übertragungsteils (R1, R2, R3, R4, R5) des Subjekts (K), durch das der von der Röntgenbildungseinheit (12) erfasste Röntgenstrahlenfluss (L) verläuft;

einen Schlitz (13) zum Beschränken eines Bereichs eines von der Röntgenquelle (11a) projizierten Röntgenstrahls, der angeordnet ist, um der Röntgenbildungseinheit (12) über die Erstreckung des Subjekts (K) zugewandt zu sein; und einen Steuerungsabschnitt (8) zum Steuern des Betriebs der Drehantriebseinheit (3) und der Verschiebeeinheit (7), wobei der Steuerungsabschnitt (8) derart konfiguriert ist, dass er die Erfassung des Röntgenstrahlenflusses (L), der durch das Subjekt (K) verläuft, durch die Röntgenbildungseinheit (12) durchführt, während er gleichzeitig das Drehen der Röntgenquelle (11a) und der Röntgenbildungseinheit (12) um das Subjekt (K) durch Drehen des Tragelements (11b) durch Betreiben der Drehantriebseinheit (3) und das Verschieben des Übertragungsteils des Subjekts (K), durch den der von der Röntgenbildungseinheit (12) erfasste Röntgenstrahlenfluss (L) verläuft, durch Betreiben der Verschiebeeinheit (6) durchführt, **dadurch gekennzeichnet, dass** die Verschiebeeinheit (7) eine Linearbewegungseinheit (70) ist, die am Tragelement (11b) angeordnet ist, um die Röntgenbildungseinheit (12) linear zu bewegen, die Linearbewegungseinheit (70) mit einer Führungsschiene (71), die entlang einer Richtung der linearen Bewegung angeordnet ist, einer Halterung (72), die hin- und herbewegbar entlang der Führungsschiene (71) befestigt ist, einem Mutterabschnitt (73), der an der Halterung (72) befestigt ist, einem Schraubenelement (74) mit Außengewinde, das in den Mutterabschnitt (73) eingeschraubt ist, und einer Drehantriebseinheit für das Schraubenelement mit Außengewinde, wie einem Servomotor, die das Schraubenelement (74) mit Außengewinde drehend antreibt, bereitgestellt wird; eine Linearbewegungseinheit (75) zum linearen Bewegen des Schlitzes (13), wobei die Linearbewegungseinheit (75) direkt an einem Dreharm oder durch ein Tragelement (11b) angeordnet ist, wobei der Dreharm (32) von der Drehantriebseinheit (3) gedreht werden kann und eine Mittelachse (C2) zur bogenförmigen Bewegung aufweist; wobei die Linearbewegungseinheit (75) zum linearen Bewegen des Schlitzes (13) mit einer Führungsschiene (76), einer Halterung (77), einem Mutterabschnitt (78), einem Schraubenelement (79) mit Außengewinde und einer Drehantriebseinheit für das Schraubenelement mit Außengewinde, wie einem Servomotor, die das Schraubenelement (79) mit Außengewinde drehend antreibt, bereitgestellt wird, wobei die Linearbewegungseinheit (70) und die Linearbewegungseinheit (75) so gesteuert werden können, dass sie sich synchron zueinander bewegen.

4. Die Röntgenbildgebungsanordnung (1a, 1b) nach einem der vorhergehenden Ansprüche, wobei der Steuerungsabschnitt (8) den Betrieb der Drehantriebseinheit (3) und der Verschiebeeinheit (6, 7) derart steuert, dass benachbarte Übertragungsteile, durch die der Röntgenstrahlenfluss (L) verläuft, an den zwei Zeitpunkten, bevor und nachdem das Tragelement (11b) einmal gedreht wird, miteinander in Kontakt stehen.

Revendications

1. Un dispositif d'imagerie à rayons X (1a), comprenant:

une source de rayons X (11a) destinée à irradier un sujet (K) par un flux de rayons X (L);
une unité d'imagerie à rayons X (12) destinée à détecter le flux de rayons X (L) traversant le sujet (K);

un élément de support (11b) destiné à supporter la source de rayons X (11a) et l'unité d'imagerie à rayons X (12);

une unité d'entraînement en rotation (3) destinée à tourner la source de rayons X (11a) et l'unité d'imagerie à rayons X (12) autour du sujet (K) en tournant l'élément de support (11b);

une unité de déplacement (6) destinée à déplacer une partie de transmission (R1, R2, R3, R4, R5) du sujet (K) par laquelle passe le flux de rayons X (L) détecté par l'unité d'imagerie à rayons X (12); et

une section de commande (8) destinée à commander l'opération de l'unité d'entraînement en rotation (3) et de l'unité de déplacement (6), la section de commande (8) étant configurée de telle manière qu'elle effectue la détection du flux de rayons X (L) traversant le sujet (K) par l'unité d'imagerie à rayons X (12) tout en effectuant simultanément la rotation de la source de rayons X (11a) et de l'unité d'imagerie à rayons X (12) autour du sujet (K) en tournant l'élément de support (11b) par l'opération de l'unité d'entraînement en rotation (3), et tout en déplaçant la partie de transmission du sujet (K) par laquelle passe le flux de rayons X (L) détecté par l'unité d'imagerie à rayons X (12) par l'opération de l'unité de déplacement (6),

caractérisé en ce que

l'unité de déplacement est un mécanisme de déplacement de position de centre de rotation le long d'une direction circonférentielle (6) destiné à déplacer la position de centre de rotation de l'élément de support (11b) le long d'une direction circonférentielle d'un cercle ayant un centre au niveau d'un point situé sur une ligne reliant la source de rayons X (11a) à l'unité d'imagerie à

rayons X (12), l'unité de déplacement (6) étant pourvue d'une roue dentée coulissante (62) présentant une forme arquée à laquelle est fixé un arbre de liaison (61), d'un pignon (63) en prise avec la roue dentée coulissante (62), d'une unité d'entraînement en rotation de pignon (64), comme un servomoteur, destinée à entraîner en rotation le pignon (63), et d'un élément de guidage (65) destiné à guider le déplacement dirigé circonférentiellement de la roue dentée coulissante (62), l'arbre de liaison (61) étant fixé à la surface supérieure d'un bras rotatif (32) pouvant être tourné par l'unité d'entraînement en rotation (3) et ayant un axe central de déplacement arqué (C2),

un arbre rotatif (31) étant fixé à la partie supérieure de l'unité de déplacement (6), des dents intérieures étant formées dans la roue dentée coulissante (62), l'axe central de déplacement arqué (C2) en présentant le centre, de sorte que, dans l'unité de déplacement (6), le pignon (63) est tourné par l'opération de l'unité d'entraînement en rotation du pignon (64), et la force d'engrenage déplaçant la roue dentée coulissante (62) de sorte que l'arbre de liaison (61) puisse être déplacé le long de la direction circonférentielle d'un cercle présentant un rayon (r), l'axe central de déplacement arquée (C2) en présentant le centre;

une rainure de guidage (66) destinée à guider le mouvement de l'arbre de liaison (61).

2. Le dispositif d'imagerie à rayons X (1a) selon la revendication 1, dans lequel une fente (13) destinée à restreindre une plage d'un rayon X projeté à partir de la source de rayons X (11a) est disposée de manière à faire face à l'unité d'imagerie à rayons X (12) sur l'étendue du sujet (K).

3. Un dispositif d'imagerie à rayons X (1b),
une source de rayons X (11a) destinée à irradier un sujet (K) par un flux de rayons X (L);
une unité d'imagerie à rayons X (12) destinée à détecter le flux de rayons X (L) traversant le sujet (K);
un élément de support (11b) destiné à supporter la source de rayons X (11a) et l'unité d'imagerie à rayons X (12);
une unité d'entraînement en rotation (3) destinée à tourner la source de rayons X (11a) et l'unité d'imagerie à rayons X (12) autour du sujet (K) en tournant l'élément de support (11b);
une unité de déplacement (7) destinée à déplacer une partie de transmission (R1, R2, R3, R4, R5) du sujet (K) par laquelle passe le flux de rayons X (L) détecté par l'unité d'imagerie à rayons X (12);
une fente (13) destinée à restreindre une plage d'un rayon X projeté à partir de la source de rayons X (11a) disposée de manière à faire face à l'unité

d'imagerie à rayons X (12) sur l'étendue du sujet (K);
 et
 une section de commande (8) destinée à commander l'opération de l'unité d'entraînement en rotation (3) et de l'unité de déplacement (7),
 la section de commande (8) étant configurée de telle manière qu'elle effectue la détection du flux de rayons X (L) traversant le sujet (K) par l'unité d'imagerie à rayons X (12) tout en effectuant simultanément la rotation de la source de rayons X (11a) et de l'unité d'imagerie à rayons X (12) autour du sujet (K) en tournant l'élément de support (11b) par l'opération de l'unité d'entraînement en rotation (3), et tout en déplaçant la partie de transmission du sujet (K) par laquelle passe le flux de rayons X (L) détecté par l'unité d'imagerie à rayons X (12) par l'opération de l'unité de déplacement (7),

caractérisé en ce que

l'unité de déplacement (7) est une unité de déplacement linéaire (70) disposée au niveau de l'élément de support (11b) afin de déplacer linéairement l'unité d'imagerie à rayons X (12),

l'unité de déplacement linéaire (70) est pourvue d'un rail de guidage (71) disposé le long d'une direction de déplacement linéaire, d'un organe de retenue (72) attaché de manière à être mobile en va-et-vient le long du rail de guidage (71), d'une section d'écrou (73) fixée à l'organe de retenue (72), d'un élément de vis mâle (74) mis en prise par vissage avec la section d'écrou (73), et d'une unité d'entraînement en rotation de l'élément de vis mâle, comme un servomoteur, qui entraîne en rotation l'élément de vis mâle (74);

une unité de déplacement linéaire (75) destinée à déplacer linéairement ladite fente (13), l'unité de déplacement linéaire (75) étant disposée directement sur un bras rotatif (32) ou par un élément de support (11b), le bras rotatif (32) pouvant être tourné par l'unité d'entraînement en rotation (3) et ayant un axe central de déplacement arqué (C2);

l'unité de déplacement linéaire (75) destinée à déplacer linéairement la fente (13) étant pourvue d'un rail de guidage (76), d'un organe de retenue (77), d'une section d'écrou (78), d'un élément de vis mâle (79), et d'une unité d'entraînement en rotation de l'élément de vis mâle, comme un servomoteur, qui entraîne en rotation l'élément de vis mâle (79), l'unité de déplacement linéaire (70) et l'unité de déplacement linéaire (75) pouvant être commandées de manière à se déplacer en synchronisation l'une avec l'autre.

4. Le dispositif d'imagerie à rayons X (1a, 1b) selon l'une des revendications précédentes, dans lequel la section de commande (8) commande l'opération de l'unité d'entraînement en rotation (3) et de l'unité de déplacement (6, 7) de telle manière que des parties de transmission adjacentes par lesquelles passe

le flux de rayons X (L) soient en contact les unes avec les autres aux deux instants avant et après que l'élément de support (11b) soit tourné une fois.

FIG. 1

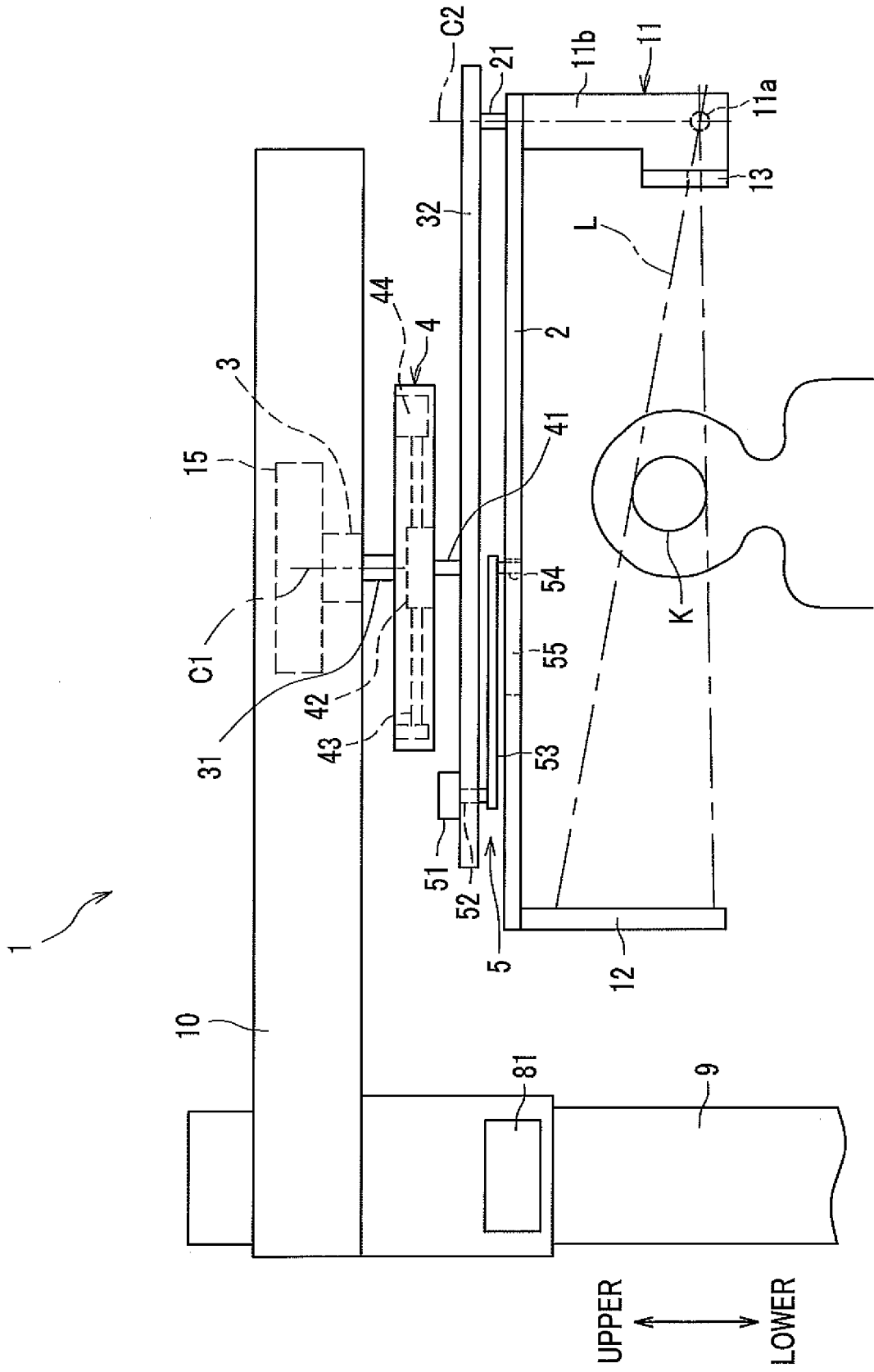


FIG. 2

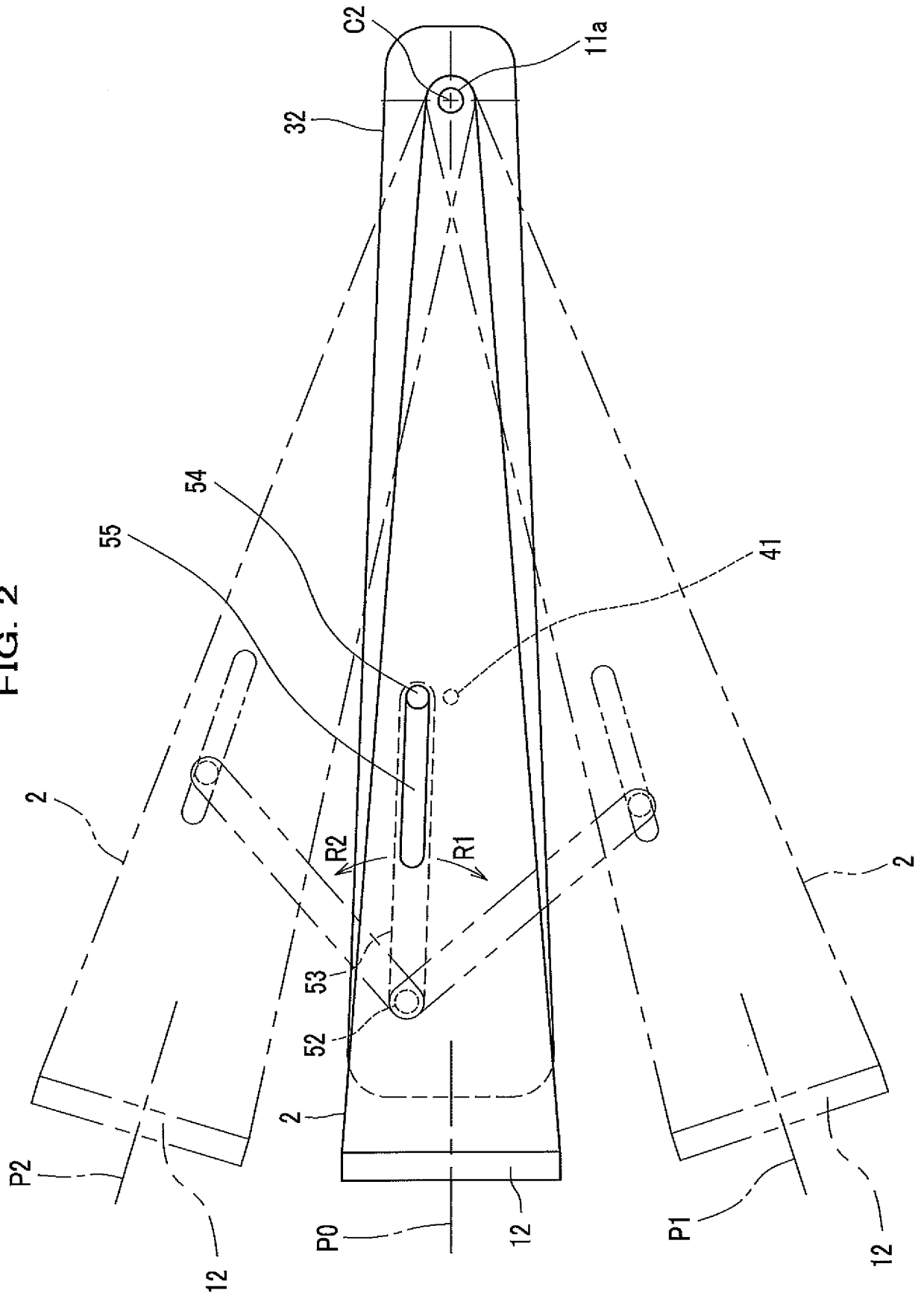


FIG. 3

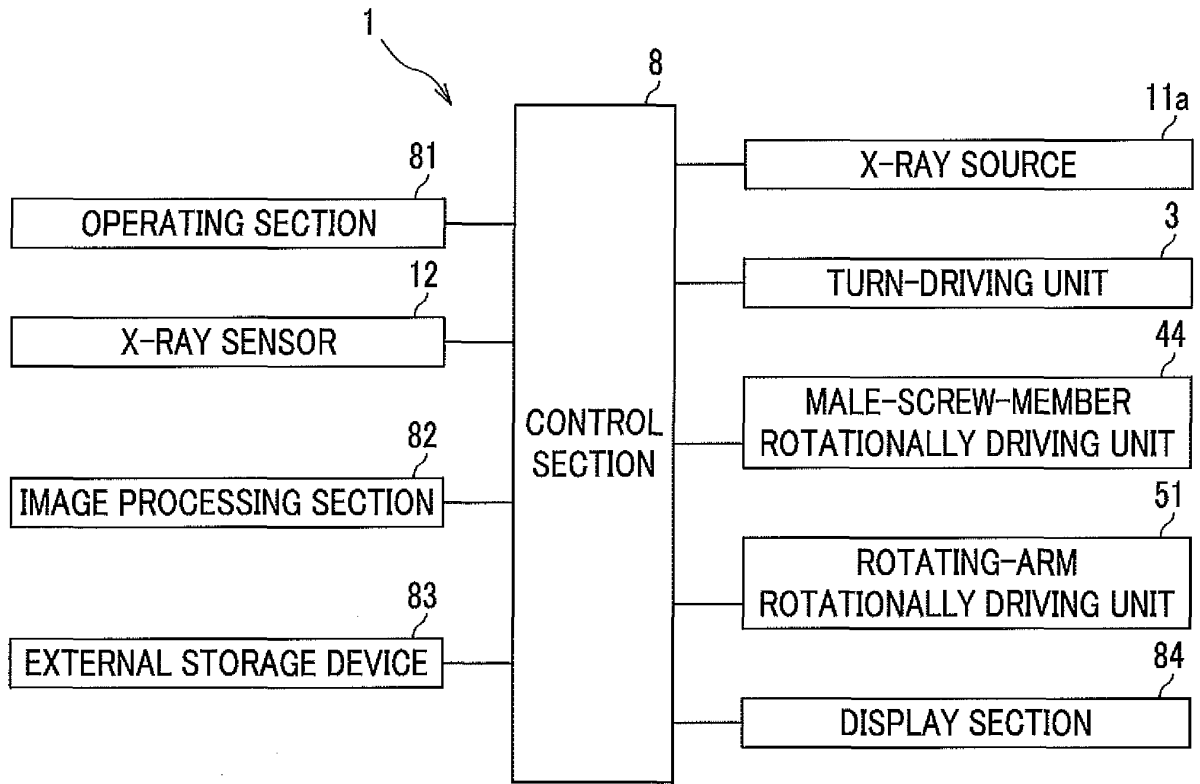


FIG. 4

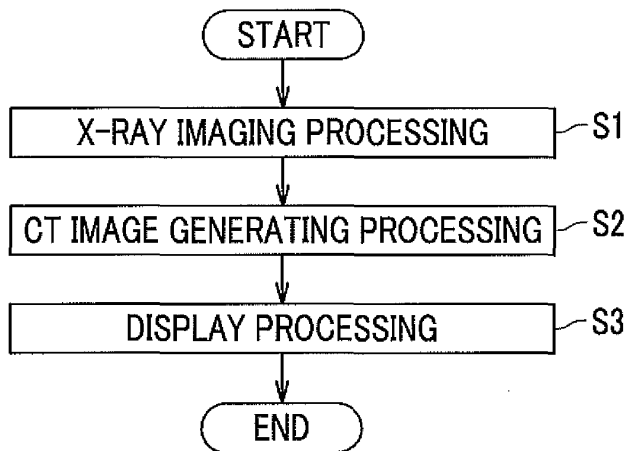


FIG. 5

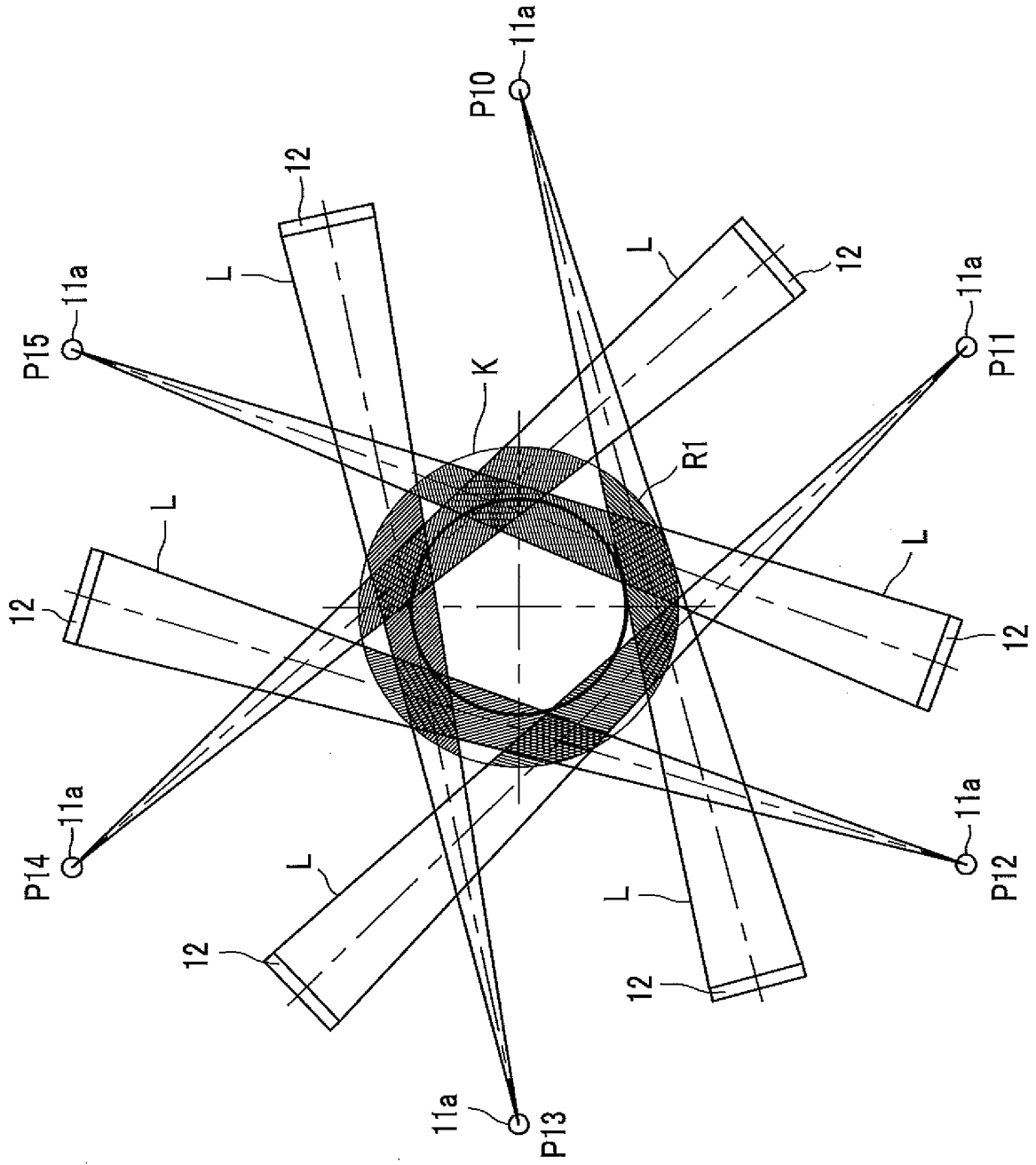


FIG. 6

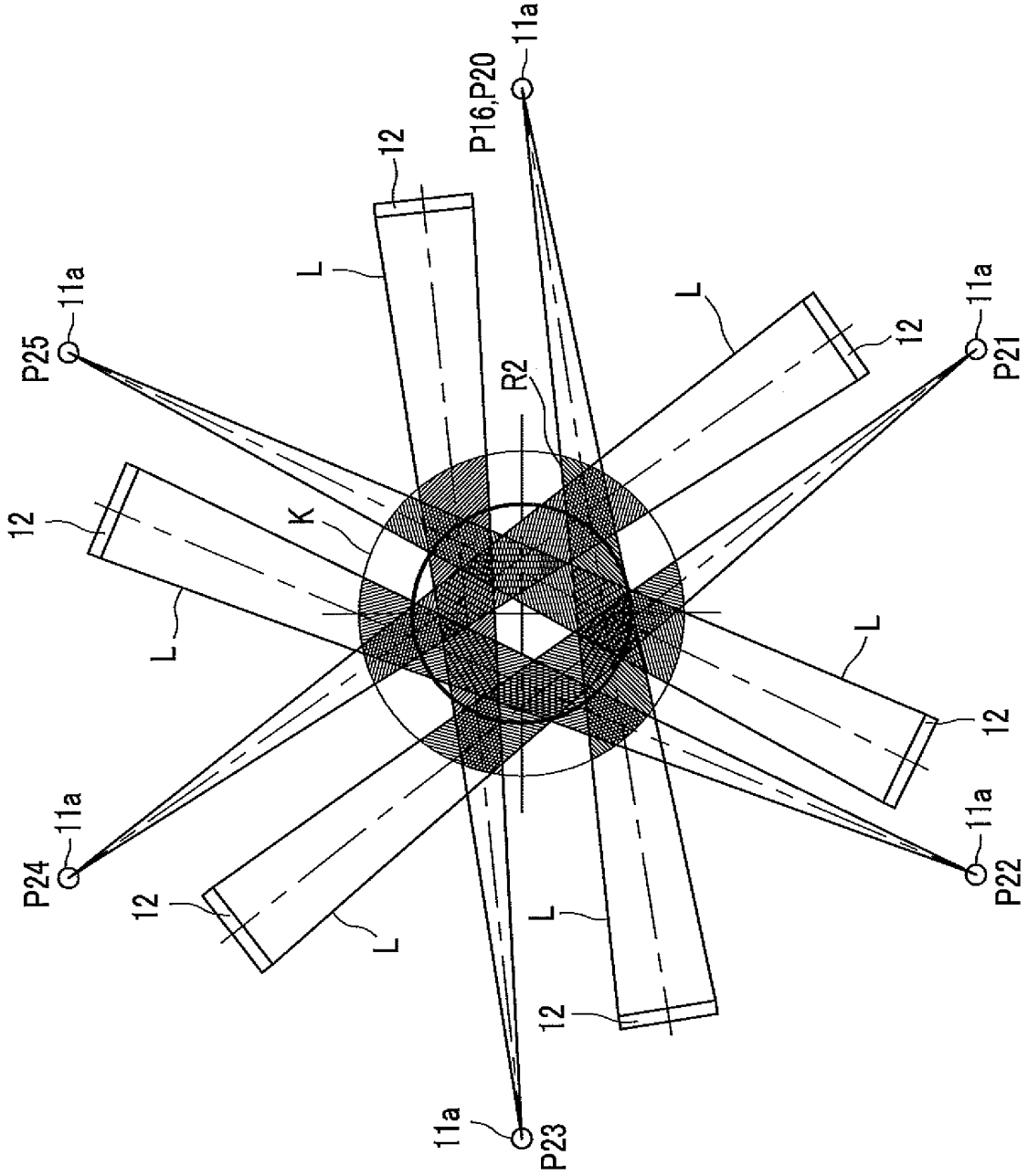


FIG. 7

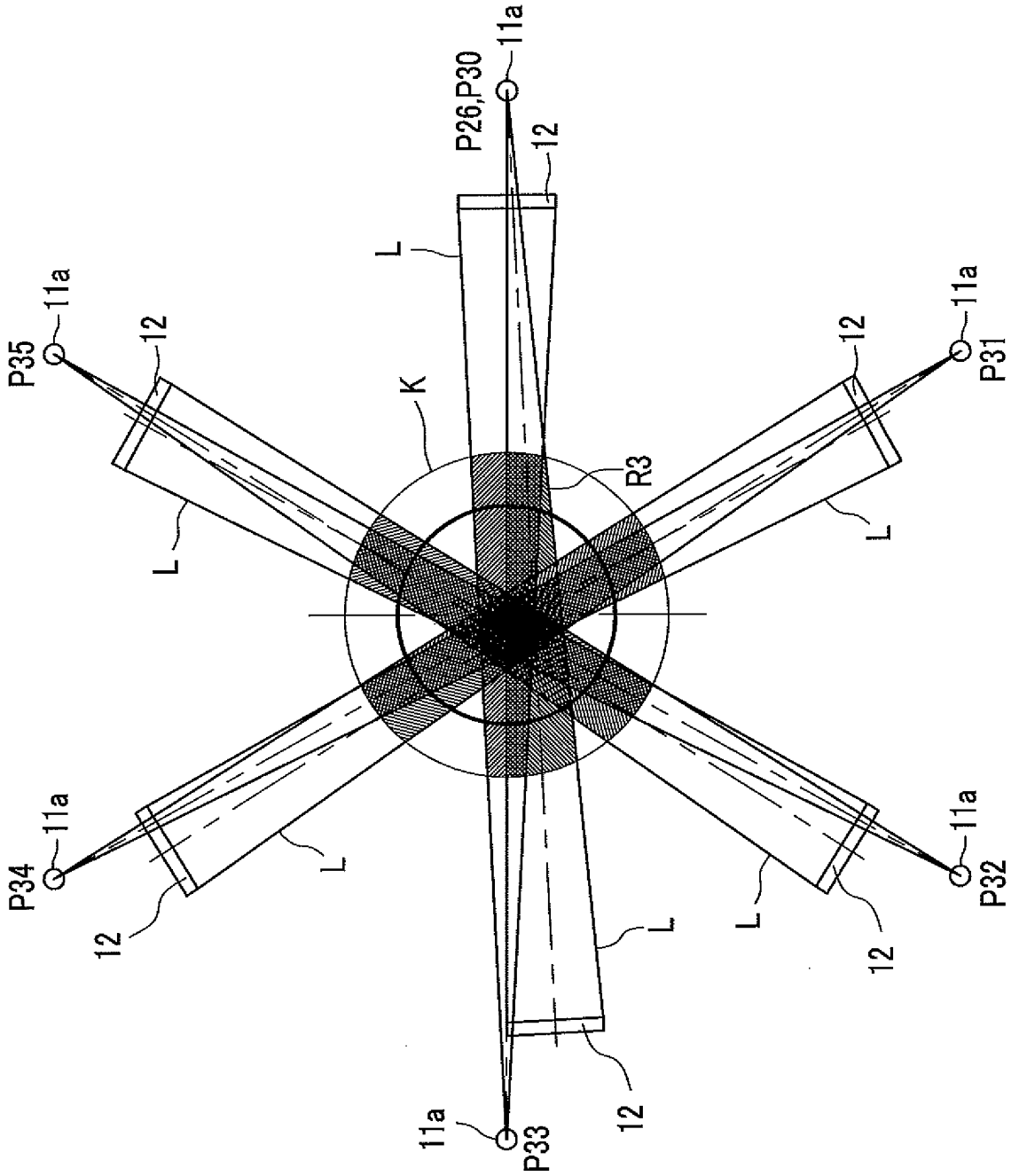


FIG. 8

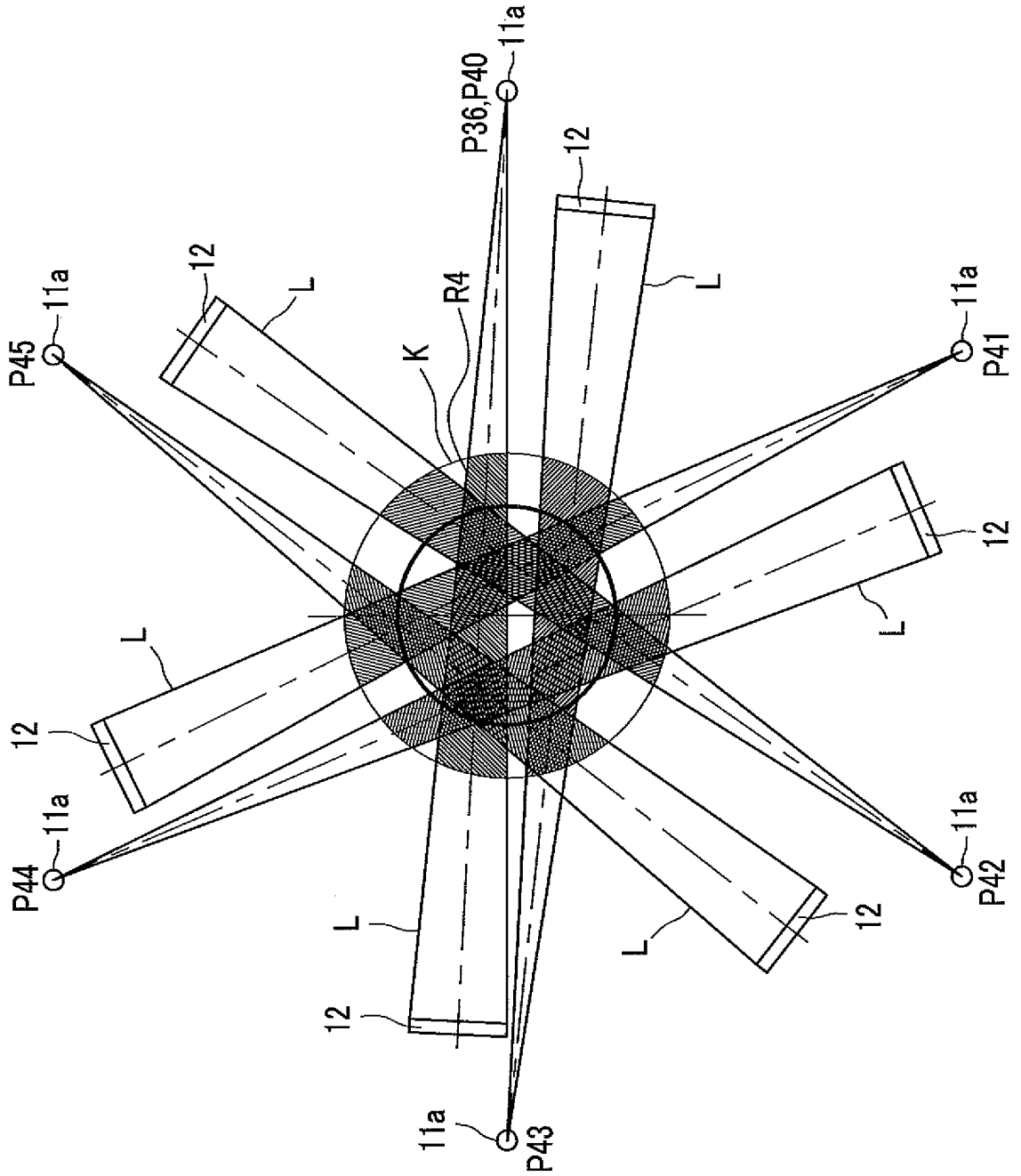


FIG. 9

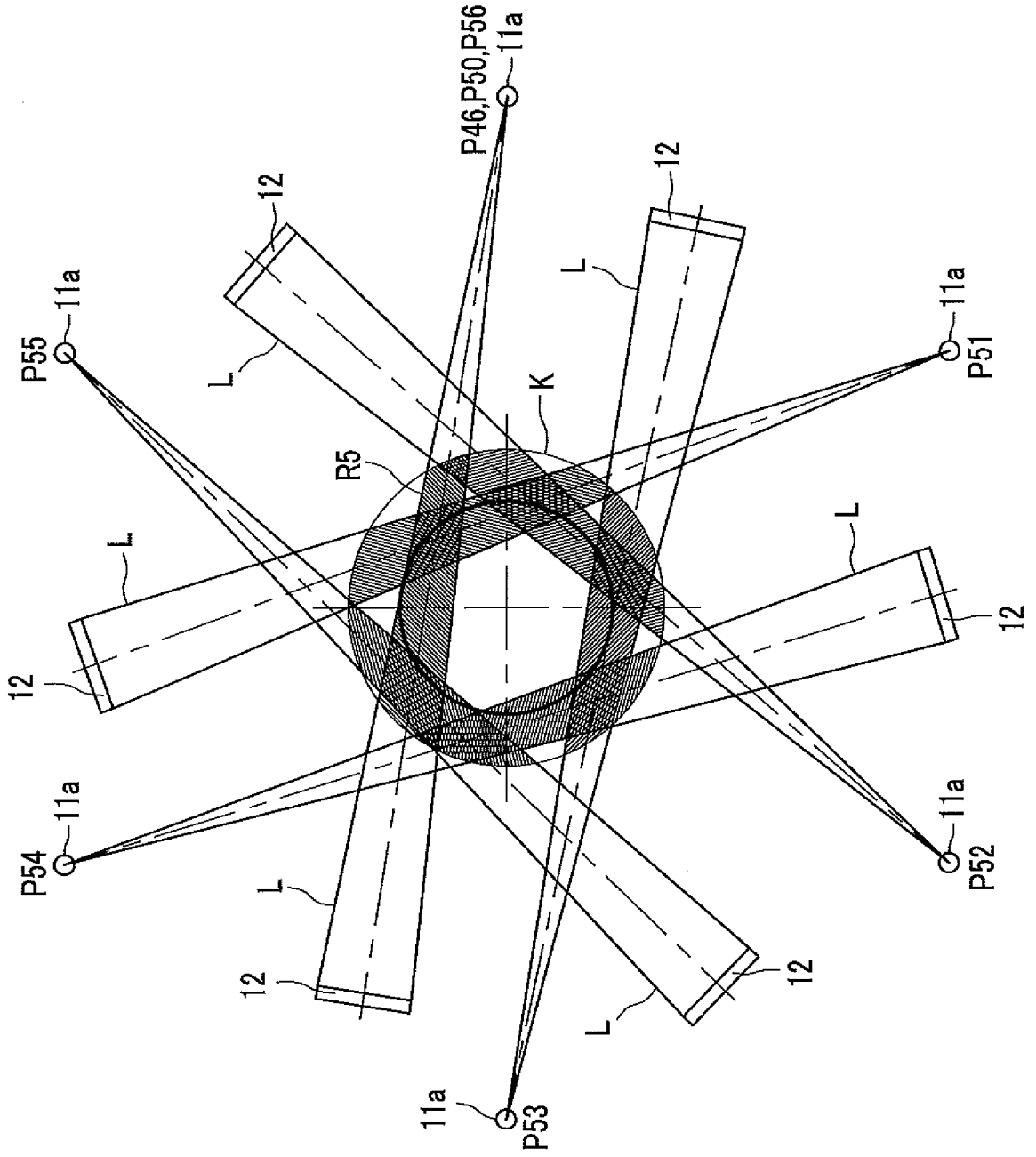


FIG. 10

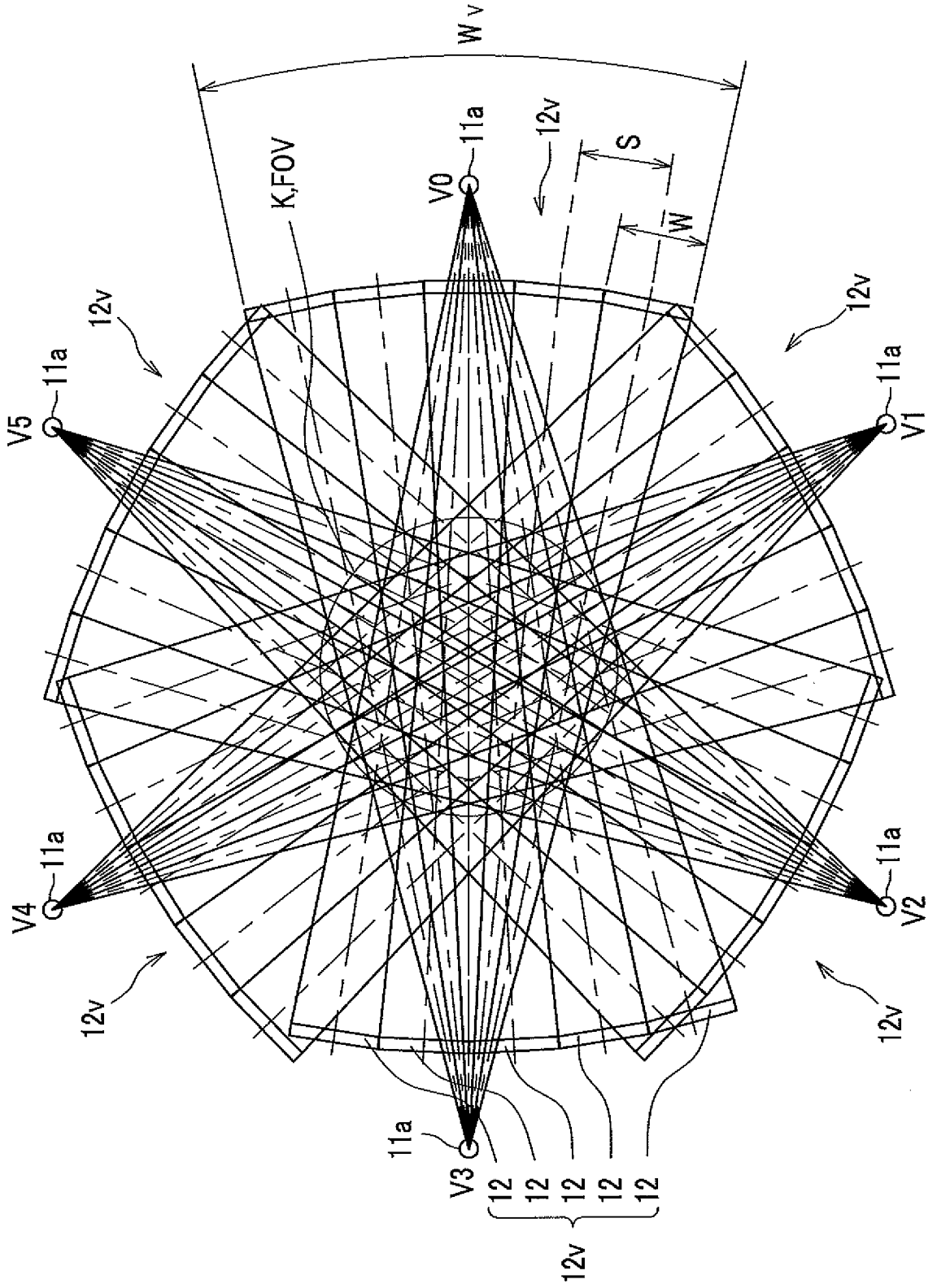


FIG. 11

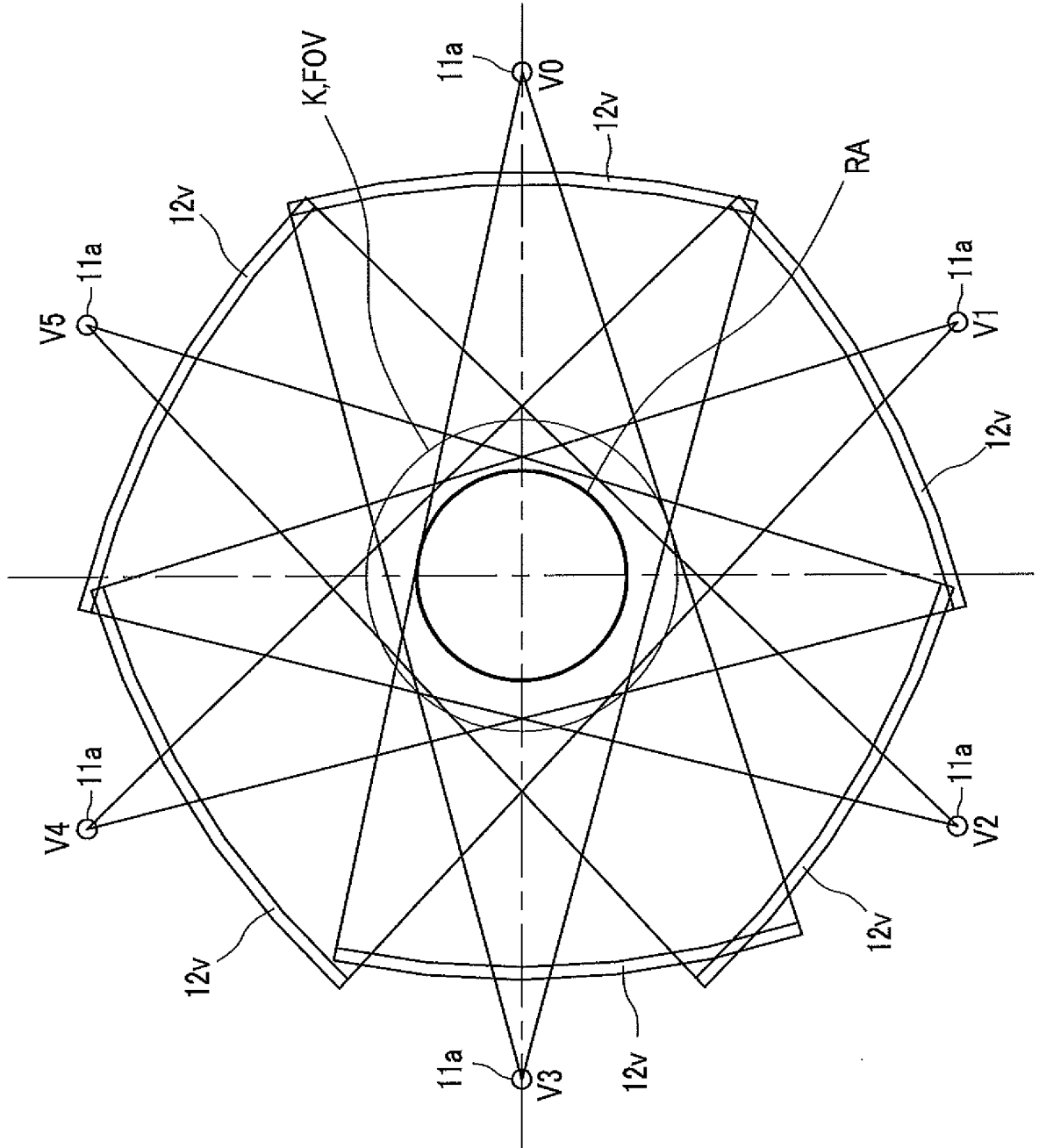


FIG. 12

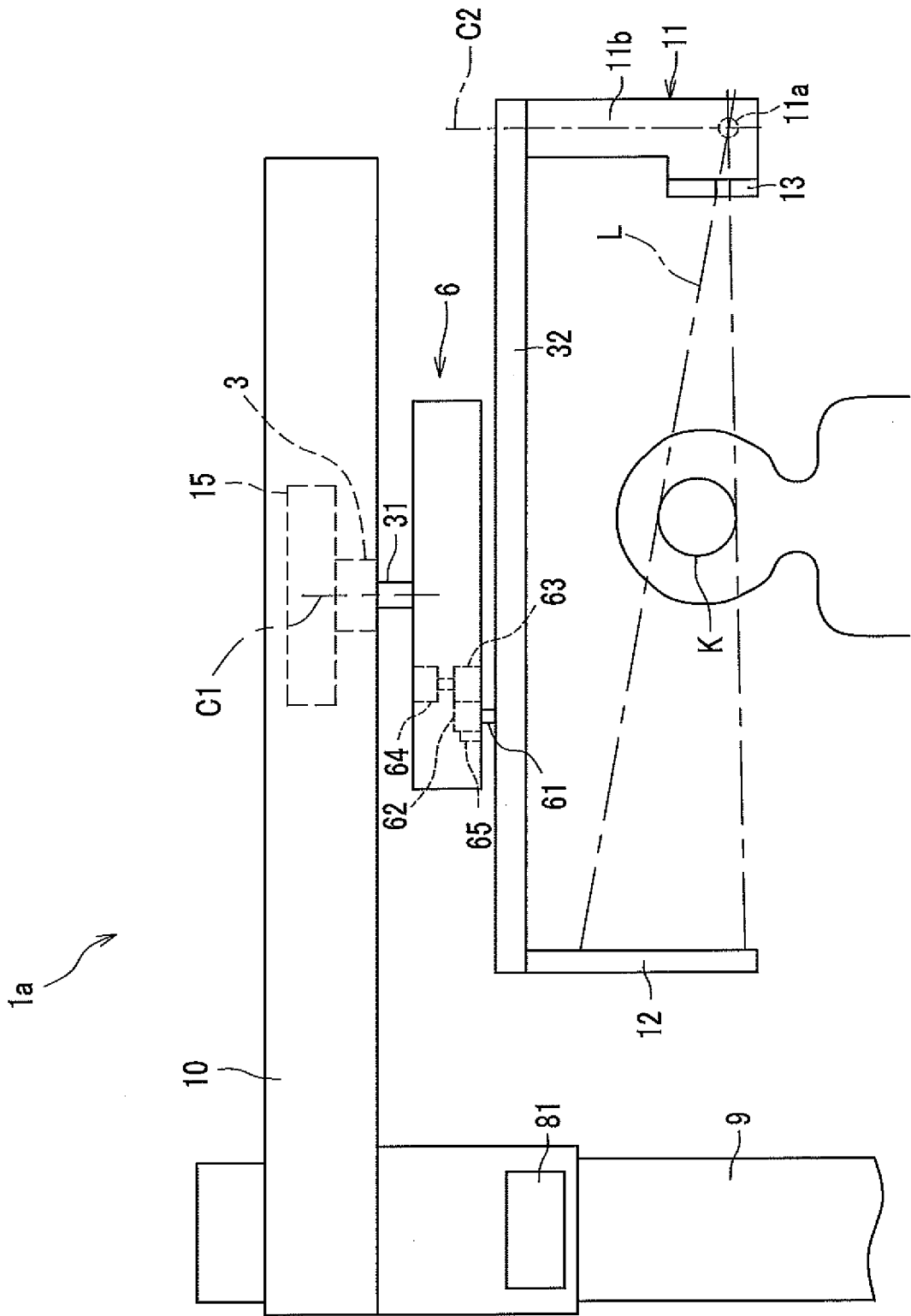


FIG. 13

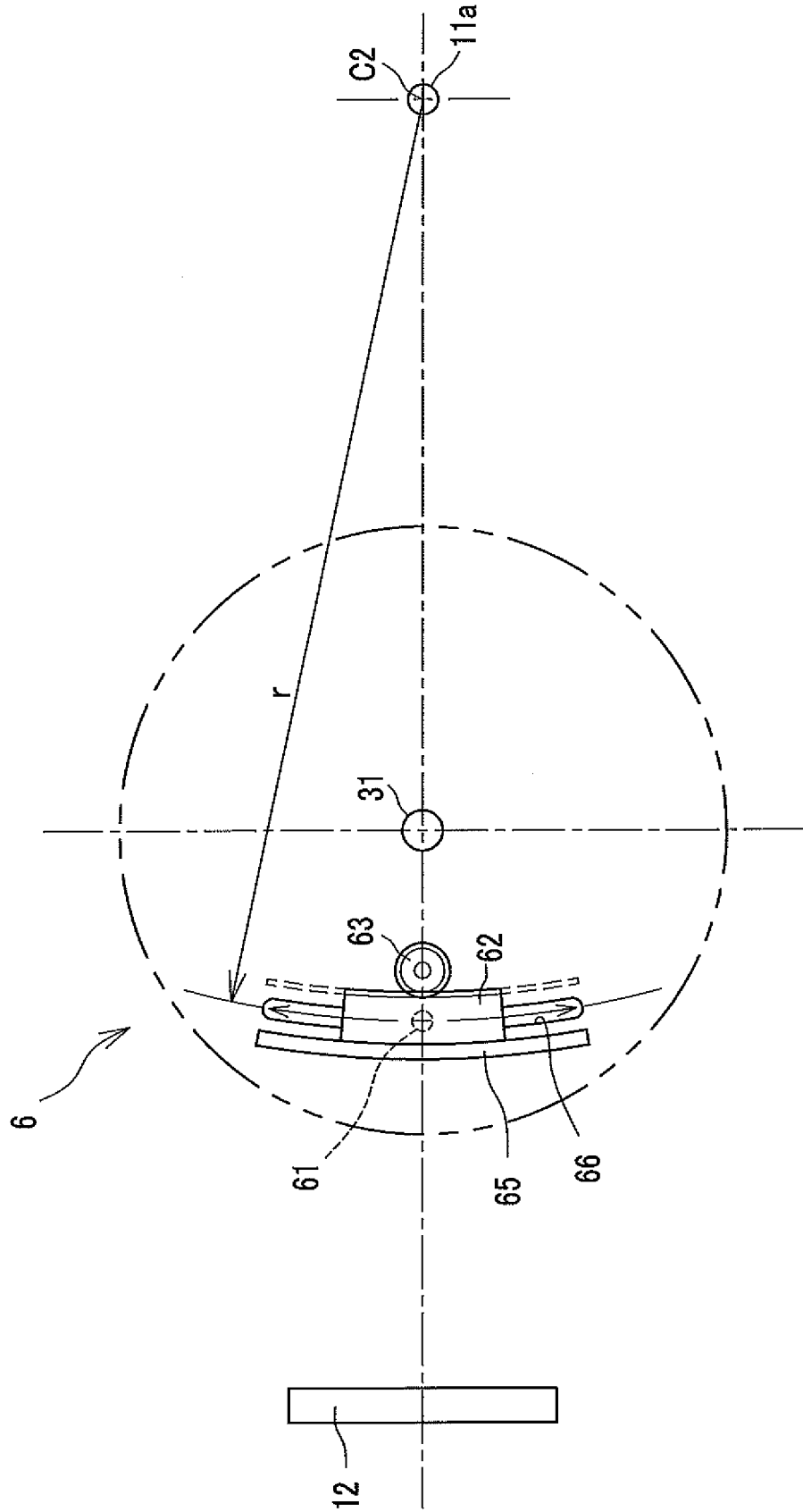


FIG. 14

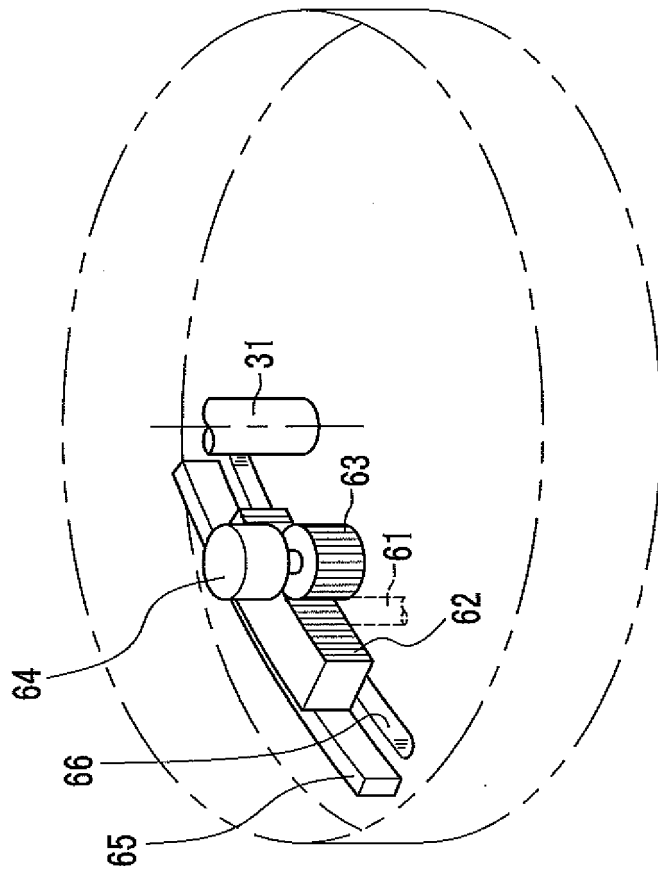
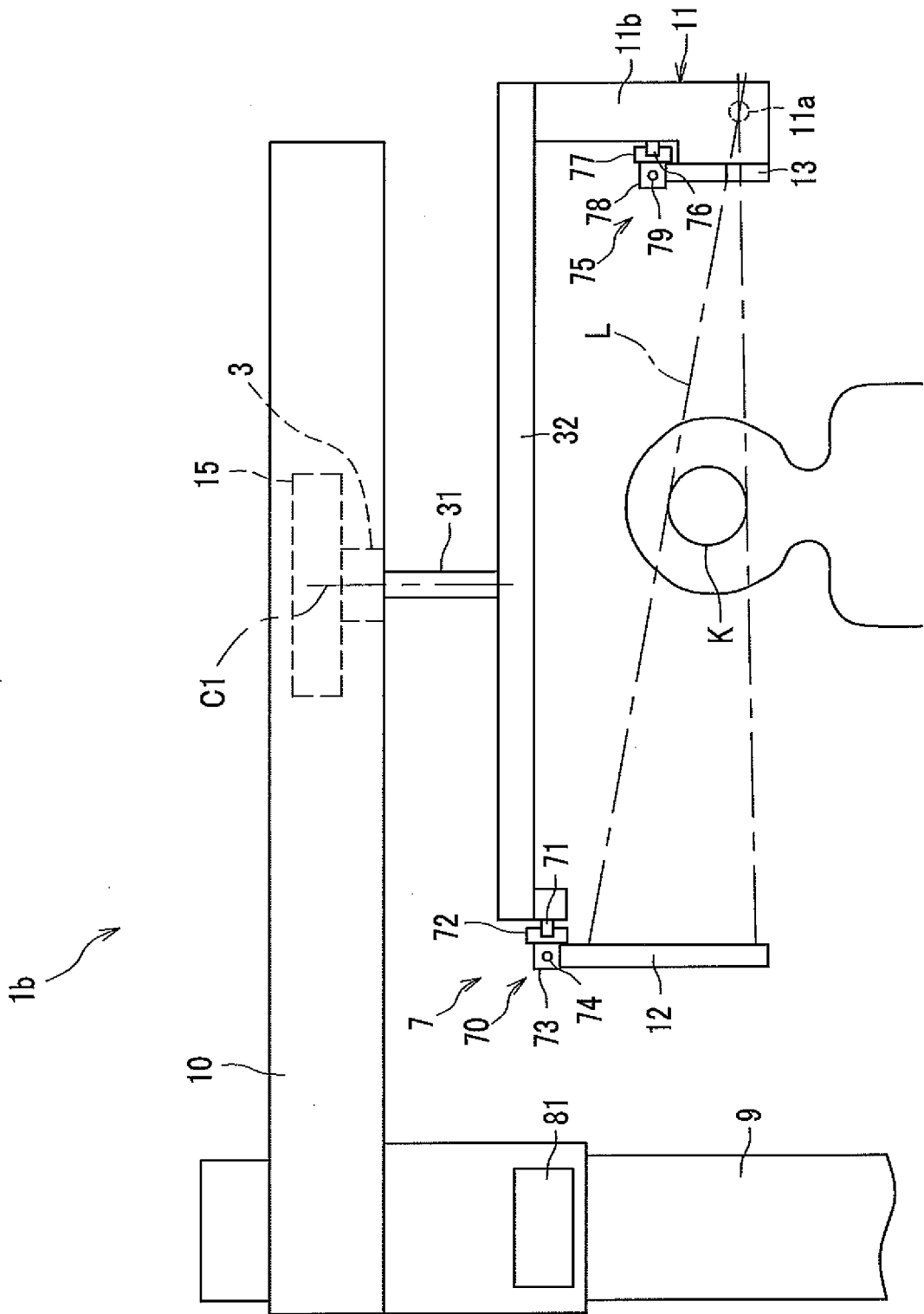


FIG. 15



REFERENCES CITED IN THE DESCRIPTION

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